

1 **Extracellular Matrix Production by Nucleus Pulposus and Bone Marrow**  
2 **Stem Cells in Response to Altered Oxygen and Glucose Microenvironments**

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10 Running Header: Matrix Production by Nucleus Pulposus and Bone Marrow Stem Cells

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20 **Abstract**

21 Bone marrow (BM) stem cells may be an ideal source of cells for intervertebral disc (IVD)  
22 regeneration. However the harsh biochemical microenvironment of the IVD may  
23 significantly influence the biological and metabolic vitality of injected stem cells and impair  
24 their repair potential. This study investigated the viability and production of key matrix  
25 proteins by nucleus pulposus (NP) and BM stem cells cultured in the typical biochemical  
26 microenvironment of the IVD consisting of altered oxygen and glucose concentrations.  
27 Culture expanded NP cells and BM stem cells were encapsulated in 1.5% alginate and  
28 ionically crosslinked to form cylindrical hydrogel constructs. Hydrogel constructs were  
29 maintained under different glucose concentrations (1mM, 5mM and 25mM) and external  
30 oxygen concentrations (5% and 20%). Cell viability was measured using the Live/Dead®  
31 assay and the production of sulphated glycosaminoglycans (sGAG) and collagen was  
32 quantified biochemically and histologically. For BM stem cells, IVD-like micro-  
33 environmental conditions (5mM glucose and 5% oxygen) increased the accumulation of  
34 sGAG and collagen. In contrast, low glucose conditions (1mM glucose) combined with 5%  
35 external oxygen concentration promoted cell death inhibiting proliferation and the  
36 accumulation of sGAG and collagen. NP-encapsulated alginate constructs were relatively  
37 insensitive to oxygen concentration or glucose condition in that they accumulated similar  
38 amounts of sGAG under all conditions. Under IVD-like microenvironmental conditions, NP  
39 cells were found to have a lower glucose consumption rate compared to BM cells and may in  
40 fact be more suitable to adapt and sustain the harsh microenvironmental conditions.  
41 Considering the highly specialised microenvironment of the central NP, these results indicate  
42 that IVD-like concentrations of low glucose and low oxygen are critical and influential for  
43 the survival and biological behaviour of stem cells. Such findings may promote and  
44 accelerate the translational research of stem cells for the treatment of IVD degeneration.

45 **Keywords:** intervertebral disc; nucleus pulposus; bone marrow; stem cells; oxygen; glucose;  
46 microenvironment; metabolism

## 47 **Introduction**

48 Low back pain (LBP) is a significant epidemiological problem and economic burden  
49 worldwide (Hoy et al., 2010). It is established that the primary cause of LBP is  
50 degeneration of the intervertebral disc (IVD) characterised by decreased extracellular matrix  
51 (ECM) synthesis and increased cell death (Deyo and Weinstein, 2001). IVD degeneration  
52 initiates within the nucleus pulposus (NP) and progresses with attrition of the annulus  
53 fibrosus (AF) which leads to eventual impairment of the IVD.

54 Healthy NP tissue contains randomly organized collagen types II and VI, embedded  
55 in a highly hydrated gel-like matrix rich in proteoglycans (PGs), with aggrecan being  
56 predominantly abundant (Inoue, 1981). Other proteoglycans such as biglycan, decorin, and  
57 fibromodulin are also present (Singh et al., 2009). The high osmotic pressure within the NP,  
58 provided by the proteoglycans, is important in maintaining tissue hydration and resisting  
59 compressive forces during normal motion and activities. As degeneration progresses, the  
60 proteoglycan content of the NP diminishes resulting in decreased osmotic pressure with a  
61 concomitant loss of hydration and reduction in disc height thereby impairing the mechanical  
62 functionality of the IVD. Synthesis and composition of collagens also vary with progressive  
63 degeneration; with increased collagen type I produced in the NP, leading to a fibrotic  
64 transformation of the NP tissue and a progressive inability to identify a clear demarcation  
65 between the NP and AF tissues. Concomitant with matrix degradation and reduced disc  
66 height is often an in-growth of blood vessels and nerves into the normally avascular and  
67 aneural tissue (Freemont et al., 1997).

68 Cell based therapies targeted to regenerate the NP region may prevent progressive  
69 degeneration. Autologous Disc Cell Transplantation (ADCT) is a therapy that involves  
70 harvesting NP tissue from the patient, isolating and expanding cells to required numbers and  
71 injecting the expanded cells into the central NP region of an early-stage degenerated IVD  
72 (Hohaus et al., 2008). However, limitations with this approach include the low yield of  
73 healthy NP cells obtainable from degenerated discs and the limited expansion capability of  
74 NP cells (Hiyama et al., 2008, Xia et al., 2013). This has motivated the exploration of stem  
75 cells due to their propensity to proliferate and their ability to form multiple tissue types  
76 (Caplan, 1991).

77 BM stem cells possess significant potential and perhaps provide a clinically feasible  
78 source of cells to promote the repair of NP tissue. The rationale and benefits to transplanting  
79 stem cells into the IVD are twofold; firstly, transplanted stem cells may stimulate endogenous  
80 NP cells, and secondly the resident host NP cells may promote differentiation of the  
81 transplanted stem cells towards a nucleus pulposus phenotype (Miyamoto et al., 2010,  
82 Richardson et al., 2006). In vivo studies have shown that implantation of stem cells into  
83 experimentally induced degenerate animal discs leads to improved disc height and  
84 accumulation of proteoglycans (Risbud et al., 2004a, Crevensten et al., 2004, Sakai et al.,  
85 2003). Furthermore, a human clinical study performed by Orozco et al injected autologous  
86 bone marrow stem cells into the nucleus pulposus of ten patients diagnosed with lumbar disc  
87 degeneration. Results indicated that pain, disability, and quality of life improved over the 12  
88 month trial (Orozco et al., 2011).

89 However, the regenerative potential of BM stem cells may be limited by the harsh  
90 microenvironment within the disc, characterised by low oxygen, low glucose and low pH  
91 conditions (Urban, 2002, Grunhagen et al., 2006, Bartels et al., 1998). In the central nucleus  
92 pulposus the oxygen concentration ranges from 5% to as low as 1% (Mwale et al., 2011), the

93 pH ranges from 7.1 to as low 6.5 (Urban, 2002) and the glucose concentration ranges from  
94 5mM to lower levels (Bibby et al., 2005) as the degeneration transgresses from mildly  
95 degenerated to a severely degenerated state. NP cells have been shown to be well adapted to  
96 this harsh microenvironment (Risbud et al., 2006), but this biochemical microenvironment  
97 may negatively influence the biological and metabolic vitality of stem cells and impair their  
98 regeneration potential. Therefore, understanding how stem cells respond to limited nutrient  
99 availability is a key factor for clinical translation.

100         Numerous studies have focused on cell growth and survival (Johnson et al., 2008,  
101 Stephan et al., 2011). Stephan *et al* cultured bovine NP cells in alginate beads under zero  
102 glucose or high glucose conditions and demonstrated that NP cell proliferation and survival  
103 are influenced by the availability of glucose (Stephan et al., 2011). The absence of glucose  
104 resulted in more apoptotic and senescent cells. Interestingly, Johnson *et al* cultured bovine  
105 NP cells encapsulated in alginate gels under similar conditions and observed that glucose  
106 deprivation leads to a minimal increase in cell proliferation (Johnson et al., 2008). Mwale *et*  
107 *al* also cultured bovine NP cells encapsulated in alginate beads under different oxygen  
108 concentrations and found that low oxygen levels increased the expression of aggrecan mRNA  
109 levels but interestingly this was not reflected in GAG release (Mwale et al., 2011). Also,  
110 Stoyanov et al cultured BM stem cells in alginate beads under low and high oxygen  
111 concentrations and observed that hypoxia increased aggrecan and collagen gene expression  
112 (Stoyanov et al., 2011). Although these studies describe the influence of glucose and oxygen  
113 on NP cell and BM stem cell growth and survival, little is known of the effect on the capacity  
114 of these cells to produce NP-like matrix. Further experimentation is required to address ECM  
115 synthesis which is of major importance to the functioning of the disc. Furthermore, the same  
116 studies have investigated the effects of oxygen (Yang et al., 2013, Stoyanov et al., 2011,  
117 Risbud et al., 2006, Mwale et al., 2011) or glucose (Wuertz et al., 2008, Stephan et al., 2011,

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118 Liang et al., 2012, Deorosan and Nauman, 2011, Li et al., 2007) independently which has  
119 resulted in several contradictions in the literature and confirms the need to study the effect of  
120 combined environmental factors which more likely reflects the situation as it exists *in vivo*.

121         The objective of this study was to investigate how microenvironmental conditions  
122 may affect subsequent matrix production of porcine NP and BM stem cells encapsulated in  
123 3D alginate hydrogels cultured in three different glucose (1mM, 5mM and 25mM) media at  
124 two different oxygen concentrations (5% and 20%).

125 **Methods**

126 *Nucleus Pulposus and Bone Marrow Stem Cell Isolation and Culture*

127 NP cells were harvested from the intervertebral discs (IVDs) of porcine donors (N=2, 3-4  
128 months, 20-30kg) within three hours of sacrifice as previously described (Naqvi and Buckley,  
129 2014). NP tissue was isolated and enzymatically digested in 2.5mg/ml pronase solution for 1  
130 hour followed by 3 hours in 0.5mg/ml collagenase solution at 37°C. Digested tissue/cell  
131 suspension was passed through a 100µm cell strainer to remove tissue debris followed by 70  
132 µm and 40 µm cell strainers to separate notochordal cells (NC) from the desired nucleus  
133 pulposus cells (NP) as previously described (Spillekom et al., 2014). Cells were washed three  
134 times by repeated centrifugation (650G for 5 minutes), plated at a density of  
135  $5 \times 10^3$  cells/cm<sup>2</sup> and cultured to passage 2 in T-175cm<sup>2</sup> flasks with low-glucose Dulbecco's  
136 modified eagles medium (LG-DMEM, 1mg/ml D-Glucose), supplemented with 10% Foetal  
137 bovine serum (FBS), 100U/ml penicillin, 100µg/ml streptomycin, 0.25µg/ml amphotericin B,  
138 5ng/ml Fibroblast Growth Factor-2 (FGF-2; PeproTech, UK).

139 Donor matched bone marrow (BM) was isolated from the femora and plated at  
140  $10 \times 10^6$  cells in T-75cm<sup>2</sup> flasks to allow for colony formation (P0) in supplemented LG-  
141 DMEM. After P0, cells were re-plated at  $5 \times 10^3$  cells/cm<sup>2</sup> and expanded to P2 in a humidified  
142 atmosphere at 37°C and 5% CO<sub>2</sub>. The differentiation capacity of BM cells from donors was  
143 assessed as previously described (Vinardell et al., 2011). In all cases BM stem cells  
144 demonstrated successful differentiation towards the osteogenic, adipogenic and chondrogenic  
145 lineages.

146

147

148 *Alginate Hydrogel Encapsulation and Culture*

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149 Expanded cells (NP and BM) were encapsulated in 1.5% alginate (Pronova UP LVG, FMC  
150 NovaMatrix, Norway) at a seeding density of  $4 \times 10^6$  cells/ml and ionically crosslinked with  
151 100mM calciumchloride ( $\text{CaCl}_2$ ) for 30 minutes to form cylindrical  
152 constructs (diameter=5mm; height=3mm). The geometric construct dimensions used in this  
153 study were based on previous work from our laboratory (Buckley et al., 2012). Constructs  
154 were maintained in 1mM, 5mM or 25mM-glucose medium consisting of DMEM  
155 supplemented with penicillin (100 U/mL)-streptomycin (100 $\mu$ g/mL), (both from GIBCO,  
156 Invitrogen, Ireland), 0.25  $\mu$ g/mL amphotericin B, 100  $\mu$ g/ml sodium pyruvate, 40  $\mu$ g/mL L-  
157 proline, 1.5 mg/mL bovine serum albumin, 4.7  $\mu$ g/mL linoleic acid, 1 $\times$  insulin–transferrin–  
158 selenium, 50  $\mu$ g/mL L- ascorbic acid-2-phosphate, 100 nM dexamethasone (all Sigma-  
159 Aldrich, Ireland) and 10 ng/mL TGF-  $\beta$ 3 (PeproTech, UK). Constructs were cultured in  
160 standard 24 well plates with one construct per well with 2mL of supplemented medium in  
161 hypoxic (5% oxygen) or normoxic (20% oxygen) conditions. Constructs were assessed at  
162 days 0 and 21 in terms of cell viability (n=1), biochemical content (DNA, sulfated-  
163 glycosaminoglycan (sGAG) and collagen content) (n=3), histologically and  
164 immunohistochemically (n=2). This study was performed twice with independent donors in  
165 each case. Results were reproducible for all conditions investigated.

166

### ***Cell Viability***

168 Cell viability was assessed using a LIVE/DEAD® Viability/Cytotoxicity Assay Kit  
169 (Invitrogen, Bio-science, Ireland). Constructs were removed from culture, sectioned, rinsed  
170 with phosphate buffered saline (PBS) and incubated for 1 hour at 37°C in live/dead solution  
171 containing 2  $\mu$ M calcein AM, 4  $\mu$ M ethidium homodimer-1 (EthD-1). After incubation  
172 segments were again washed with PBS and imaged with an Olympus FV-1000 Point-



173 Scanning Confocal Microscope (Southend-on-Sea, UK) at 515 and 615 nm channels and  
174 analysed using FV10-ASW 2.0 Viewer software.

175

#### 176 ***Quantitative Biochemical Analysis***

177 Samples were digested with papain (125µg/ml) in 0.1M sodium acetate, 5mM L-  
178 cysteine HCl, and 0.05 M EDTA (Sigma–Aldrich, Ireland) at 60°C under constant agitation  
179 for 18 hours. DNA content was quantified using the Hoescht 33258 dye-based DNA QF Kit  
180 (Sigma-Aldrich, Ireland). Proteoglycan content was quantified using the dimethylmethylen  
181 blue (DMMB) dye-binding assay (Blyscan, Biocolor Ltd, Northern Ireland) with a  
182 chondroitin sulphate standard. Total collagen content was determined by measuring the  
183 hydroxyproline content. Briefly, samples were hydrolysed at 110°C for 18 hours in  
184 concentrated hydrochloric acid (HCl) (38%) and assayed using a chloramine-T assay  
185 (Kafienah and Sims, 2004), using a hydroxyproline-to-collagen ratio of 1:7.69 (Ignat'eva et  
186 al., 2007).

187       Glucose concentrations in media samples from Day 18 to Day 21 were quantitatively  
188 measured using a glucose meter (Accu-Chek Aviva glucose meter, Roche Diagnostics Ltd,  
189 UK). Samples of culture media (1mM, 5mM and 25mM) served as controls. Cellular  
190 consumption rates were determined by normalising to cell number and time.

191

#### 192 ***Histology and Immunohistochemistry***

193 Constructs were fixed in 4% paraformaldehyde (PFA) overnight, dehydrated in ethanol,  
194 embedded in paraffin wax and sectioned at a thickness of 8 µm. Sections were stained for  
195 glycosaminoglycans (GAGs) using aldehyde fuchsin and 1% alcian blue 8GX (Sigma–  
196 Aldrich, Ireland) in 0.1M HCl (Simmons et al., 2004) and picro-sirius red to assess for

197 collagen deposition. The deposition of collagen types I and II were identified through  
198 immunohistochemistry. Briefly, sections were rinsed with PBS before treatment with  
199 chondroitinase ABC in a humidified environment at 37°C. Slides were rinsed with PBS and  
200 non-specific sites were blocked with goat serum. Sections were incubated for 1 hour at 4°C  
201 with the primary antibody; mouse monoclonal collagen type I antibody (1:200; 1 mg/ml) or  
202 mouse monoclonal anti-collagen type II (1:80; 1 mg/ml). After washing in PBS, sections  
203 were quenched of peroxidase activity and incubated for 1 hour in the secondary  
204 antibody; anti-mouse IgG biotin antibody produced in goats (1:133; 2.1 mg/ml). Colour was  
205 developed using the Vectastain ABC reagent followed by exposure to peroxidase DAB  
206 substrate kit. Positive and negative controls of porcine ligament and cartilage were included  
207 for each batch.

208

### 209 *Statistical Analyses*

210 Statistical analyses were performed using GraphPad Prism (version 4) software. Two-way  
211 ANOVA was used for analysis of variance with Bonferroni post-tests to compare  
212 between groups. Numerical and graphical results are displayed as mean  $\pm$  standard deviation.  
213 Significance was accepted at a level of  $p < 0.05$ .

214

215 **Results**

216 *Viability of Nucleus Pulposus and Bone marrow Stem Cells in IVD-*  
217 *like Microenvironmental Conditions*

218 For BM constructs, DNA content increased from day 0 for both oxygen concentrations  
219 irrespective of glucose condition (Fig 1A). A similar result was obtained for NP constructs  
220 maintained in 5mM glucose under normoxic conditions (20% oxygen). These results were  
221 confirmed through confocal imaging of live and dead cells (Figure 1B, C). Interestingly, a  
222 core of dead cells was observed in all BM constructs irrespective of the culture condition,  
223 although this core effect was more pronounced in the group maintained in 1mM glucose  
224 under hypoxia. A similar core effect was observed in NP constructs maintained in 5mM  
225 glucose in normoxia. The increase in DNA content in BM constructs from day 0 to day 21  
226 may be due to increased cell proliferation in the periphery of constructs.

227

228 *Bone Marrow Stem Cells Accumulated Greater Amounts of sGAG and Collagen in NP-like*  
229 *Microenvironmental Conditions*

230 A differential response for total sGAG content was observed for NP and BM constructs  
231 depending on oxygen concentration (Figure 2A). Under normoxic conditions, total sGAG  
232 content was significantly higher for NP compared to BM constructs. In contrast,  
233 hypoxia promoted the highest total sGAG accumulation for BM constructs maintained  
234 in IVD-like microenvironmental conditions (5mM glucose and 5% oxygen). When  
235 normalised to DNA content, NP constructs displayed similar amounts of sGAG content under  
236 all conditions which correlated highly with aldehyde fuchsin staining of the constructs where  
237 NP constructs appeared to accumulate similar amounts of sGAG irrespective of glucose  
238 condition or oxygen concentration (Figure 2B). Of note, BM constructs maintained in 1mM  
239 glucose in hypoxia accumulated sGAG in the periphery of the gel confirming the cell

240 viability results where dead cells were located in the centre of the hydrogel construct. Also,  
241 BM constructs maintained in normoxia exhibited sGAG deposition in the pericellular region  
242 only.

243 In terms of collagen accumulation NP constructs maintained in very low glucose  
244 conditions in hypoxia exhibited significantly less collagen content compared to those  
245 maintained in normoxia (Figure 3A). BM constructs maintained in 1mM glucose in normoxia  
246 demonstrated significantly higher collagen content compared with those maintained in  
247 hypoxia and similar results were obtained when collagen content was normalised to DNA.  
248 These observations correlated highly with picro-sirius red staining of constructs (Figure 3B).  
249 NP constructs accumulated limited but similar amounts of collagen irrespective of oxygen or  
250 glucose condition. Of note, BM constructs maintained in 1mM glucose and in  
251 hypoxia displayed limited collagen accumulation. Also, collagen staining of BM  
252 constructs maintained in normoxia demonstrated pericellular collagen deposition only.

253 In terms of sGAG to collagen ratio, hypoxia resulted in higher ratios for both cell  
254 types, with the highest ratios observed for NP (Figure 3C). Also, for BM constructs  
255 maintained in hypoxia, there was an ~~observed~~ decrease in sGAG:Collagen ratio with  
256 increasing glucose concentration.

257 Immunohistochemistry results revealed that BM constructs in 25mM glucose in  
258 hypoxia resulted in increased accumulation of collagen type I compared to normoxia (Figure  
259 4A). In contrast, for NP constructs under the same glucose conditions; those maintained in  
260 normoxia resulted in increased accumulation of collagen type I compared to hypoxia.

261 In terms of collagen type II deposition, BM constructs deposited greater amounts  
262 when maintained in IVD-like microenvironmental conditions (5mM glucose and 5% oxygen)  
263 with limited deposition under ischemic conditions (very low glucose and hypoxia) (Figure

264 4B). Also, NP constructs maintained in ischemic conditions (very low glucose and hypoxia)  
265 exhibited significantly less deposition of collagen type II compared to normoxia (Figure 4B).

266

267 **Glucose Consumption Rate of Bone Marrow Stem Cells in IVD-like**  
268 **Microenvironmental Conditions**

269 BM constructs maintained in IVD-like microenvironmental conditions (5mM glucose and 5%  
270 oxygen) displayed a significantly higher glucose consumption rate ( $p<0.01$ ) compared to NP  
271 constructs maintained under the same conditions. In addition, both cell types exhibited a  
272 significantly higher glucose consumption rate ( $p<0.01$ ) compared to constructs maintained in  
273 normoxic conditions (Figure 5). Interestingly, under hypoxic conditions, BM constructs  
274 maintained in very low glucose (1mM) exhibited a lower consumption rate compared to BM  
275 constructs under 5mM and 25mM glucose conditions ( $p<0.01$ ). Furthermore, under hypoxic  
276 conditions, BM constructs maintained in high glucose (25mM) exhibited a significantly  
277 higher glucose consumption rate compared to those maintained in normoxia and NP  
278 constructs irrespective of external oxygen concentration.

279 **Discussion**

280 The IVD is an avascular organ relying on diffusion of essential nutrients such as oxygen and  
281 glucose through the endplate thereby creating a challenging biochemical microenvironment.  
282 Translation of stem cell therapies into a multimodal protocol for IVD degeneration requires  
283 not only the survival of these cells but also their ability to function normally amidst the harsh  
284 microenvironment of hypoxia, low nutrition, acidic pH, high mechanical loading, high  
285 osmolarity, and a complicated protease and cytokine network (Wuertz et al., 2008, Urban,  
286 2002). In this study we investigated the influence of external oxygen concentration (5%  
287 and 20% O<sub>2</sub>) and three different glucose concentrations (1mM, 5mM and 20mM) on  
288 bone marrow (BM) stem cells and nucleus pulposus (NP) cells encapsulated in 3D alginate  
289 hydrogels.

290 We found that BM stem cells survive and synthesize appropriate matrix  
291 components such as sGAG and collagen in low external oxygen of 5% and low glucose  
292 concentration of 5mM representative of IVD microenvironmental conditions. Under the same  
293 external oxygen concentration of 5% and a very low glucose concentration (1mM), BM  
294 viability was reduced, particularly in the core region where we also observed reduced  
295 accumulation of matrix components (sGAG and collagen). Importantly, the GAG:Collagen  
296 ratio was relatively higher in BM constructs maintained in hypoxia compared to normoxia. A  
297 high GAG:collagen ratio may provide an appropriate metric of identifying an NP-like tissue  
298 type. The healthy NP contains randomly organized collagen type II (Inoue, 1981), embedded  
299 in a highly hydrated gel-like matrix rich in proteoglycans (PGs), with aggrecan being  
300 predominantly abundant resulting in a high GAG:collagen ratio. Conversely, the degenerated  
301 NP loses its proteoglycan content with synthesis and composition of collagens also varying  
302 resulting in an altered GAG:collagen ratio. If stem cells are to be differentiated towards a disc  
303 cell phenotype, it will be essential to verify that the ultimate matrix that they produce has an

304 appropriate GAG to collagen ratio which, for native NP, is approximately 3.5:1 (Mwale et al.,  
305 2004). While this ratio may not help in determining whether ultimate differentiation has  
306 occurred, it provides an indication for the correct composition of the tissue that the cells  
307 produce (Mwale et al., 2004).

308         Glucose is a source of energy that markedly affects viability, proliferation and  
309 differentiation of stem cells. It should be noted that cells were encapsulated in a 3D alginate  
310 hydrogel (3mmHx5mmØ) thus, for those gels maintained in hypoxia this 3D geometry has an  
311 effect of further reducing the oxygen concentration in the core due to cellular consumption  
312 (Buckley et al., 2012). This may explain the observed cell death due to inadequate oxygen  
313 combined with diminished glucose availability limiting homogeneous deposition of  
314 extracellular matrix which has been previously reported for bone marrow stem cells  
315 undergoing chondrogenesis (Farrell et al., 2012).

316         The results from this study illustrate that BM constructs exhibit an increased glucose  
317 consumption rate under hypoxic conditions compared to normoxic. Interestingly, the same  
318 constructs exhibit an increased glucose consumption rate compared to NP constructs under  
319 the same external oxygen tension demonstrating that NP cells consume less glucose than BM  
320 cells which suggests that NP cells can more readily adapt to changes in microenvironmental  
321 conditions. These findings provide important insight in the development of clinical cell-based  
322 therapies in determining the suitability of specific cell types for targeted regeneration.

323         Indeed, it has previously been reported that glucose uptake is increased when  
324 maintained in hypoxia and that stem cells are known to possess the ability to adapt their  
325 oxygen consumption rate to changes in the oxygen environment (Pattappa et al., 2013).  
326 Deschepper *et al* previously demonstrated that stem cells can remain viable when maintained  
327 in severe hypoxic conditions (i.e. 0.2% O<sub>2</sub>) but not in the absence of glucose (Deschepper et  
328 al., 2010). This correlates well with the results from this study where BM-encapsulated gels

329 maintained in hypoxia with sufficient glucose (5mM and 25mM) demonstrated higher cell  
330 viability, sGAG and collagen accumulation. Importantly, the reduced cell viability was not  
331 evident in BM-encapsulated alginate hydrogels maintained under the same very low glucose  
332 concentration (1mM glucose) and an external oxygen concentration of 20%. Under these  
333 conditions, cells appeared to remain viable but only deposited matrix pericellularly.  
334 Furthermore, this was observed for all BM-encapsulated alginate hydrogels maintained under  
335 20% oxygen conditions. Interestingly, the therapeutic potential of stem cells is commonly  
336 investigated under 20% O<sub>2</sub> (normoxia) conditions in vitro while the typical physiological  
337 oxygen concentration in human ranges from 4% to 7% (Packer and Fuehr, 1977, Kofoed et  
338 al., 1985) and falls to 1% in some pathological ischemic tissues, as well as in the degenerated  
339 IVD (Bartels et al., 1998). Numerous studies have investigated the influence of hypoxia and  
340 have found that BM stem cells proliferated more rapidly, exhibited greater colony forming  
341 unit (CFU) formation ability (Grayson et al., 2006, Grayson et al., 2007), and maintained  
342 better “stemness” in hypoxia through the down regulation of E2A-p21 by HIF-1a-Twist  
343 pathway (Tsai et al., 2011). Furthermore, previous studies have demonstrated that glucose is  
344 a significant factor in the metabolic response of mesenchymal stem cells (Deorosan and  
345 Nauman, 2011) and that a low oxygen environment enhances GAG synthesis in pellets and  
346 hydrogels (Sheehy et al., 2012). Risbud *et al.* found that 2% O<sub>2</sub> and 10 ng/ml TGF- $\beta$  could  
347 stimulate rat BM stem cell differentiation to acquire phenotypes similar to that of NP cells  
348 (Risbud et al., 2004b).

349 In contrast, NP-encapsulated alginate hydrogels maintained under the same very low  
350 glucose concentration (1mM glucose) and external oxygen concentration of 5% did not  
351 exhibit reduced cell viability. In fact, NP cells remained relatively insensitive to  
352 external microenvironmental conditions such that similar amounts of sGAG and collagen  
353 were homogeneously deposited throughout. This may be due to reduced glucose and oxygen



354 consumption rates as NP cells naturally reside in a microenvironment with limited nutrient  
355 availability. The cell specific response observed in this study may thus be a function  
356 of metabolic activity. It is plausible that at a particular oxygen concentration and glucose  
357 concentration, NP cells and stem cells possess altering metabolic demands. Agrawal *et al*  
358 indicated that oxygen-independent stabilization of HIF-1 $\alpha$ , a transcription factor that  
359 regulates oxidative metabolism, in NP cells is a metabolic adaptation to a unique  
360 microenvironment (Agrawal et al., 2007). Furthermore, it should be noted that these  
361 experiments were performed using a cell density of  $4 \times 10^6$  cells/ml, which is the typical cell  
362 density of native nucleus pulposus tissue. Higher seeding densities that are typically used in  
363 tissue engineering investigations would exacerbate the nutrient demands resulting in limited  
364 matrix formation. This is an important consideration for IVD regeneration strategies  
365 regarding the optimal number of cells that can be injected into the intervertebral disc to elicit  
366 a therapeutic response and formation of new tissue. The success of any cell based strategy  
367 will therefore be dependent on the state of degeneration and more importantly the  
368 microenvironment of the disc that can maintain the viability and support the function of  
369 injected cells.

370         Among several studies that have investigated the effects of IVD-like culture  
371 conditions on stem cell survival and differentiation, Weurtz *et al* demonstrated that  
372 combining low glucose with high osmolarity (485mOsm) and low pH (6.8) is detrimental to  
373 the differentiation of stem cells, with decreased cellular proliferation and collagen and sGAG  
374 expression suggesting that the beneficial effects of IVD-like low-glucose culture are not  
375 sufficient for promotion of stem cell differentiation when other environmental factors are  
376 considered (Wuertz et al., 2008). Of note this study lacks the effect of hypoxia which is  
377 known to be a potent regulator of matrix production. Furthermore, it is crucial to determine  
378 the response of stem cells to pro-inflammatory cytokines to fully elucidate how these cells

379 may respond post implantation in a degenerate IVD niche. Culture of stem cells in the  
380 presence of IL-1b significantly decreases culture pellet size, and cells produce an ECM with  
381 atypical mechanical strength and decreased expression of matrix molecules (Felka et al.,  
382 2009).

383         Considering the highly specialised microenvironment of the central NP, these results  
384 indicate that IVD-like low glucose and low oxygen are critical and influential for the survival  
385 and biological behaviour of BM stem cells. In this study, for BM constructs, glucose effects  
386 were only evident under hypoxic conditions suggesting that low oxygen is an important  
387 regulator of matrix production. Furthermore, NP cells and BM stem cells respond  
388 differentially to varying environmental conditions due to altered metabolic activity. Under  
389 IVD-like microenvironmental conditions, NP cells were found to have a lower glucose  
390 consumption rate compared to BM cells and may in fact be more suitable to sustain the harsh  
391 microenvironment that exists within the IVD. Such findings may promote and accelerate the  
392 development of clinical therapies in demonstrating the suitability of different cell types for  
393 targeted regeneration of the IVD.

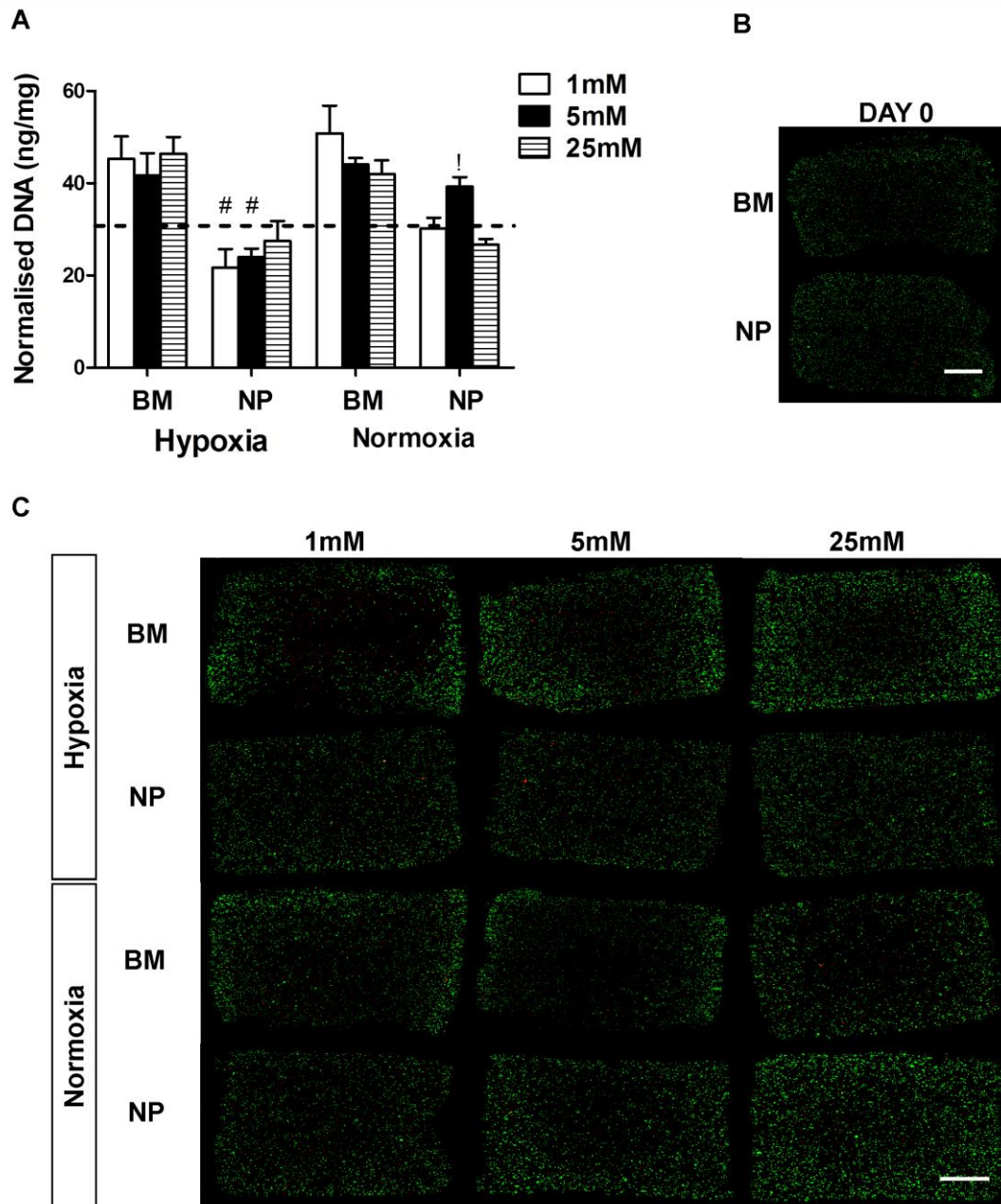
394

#### 395 **Acknowledgements**

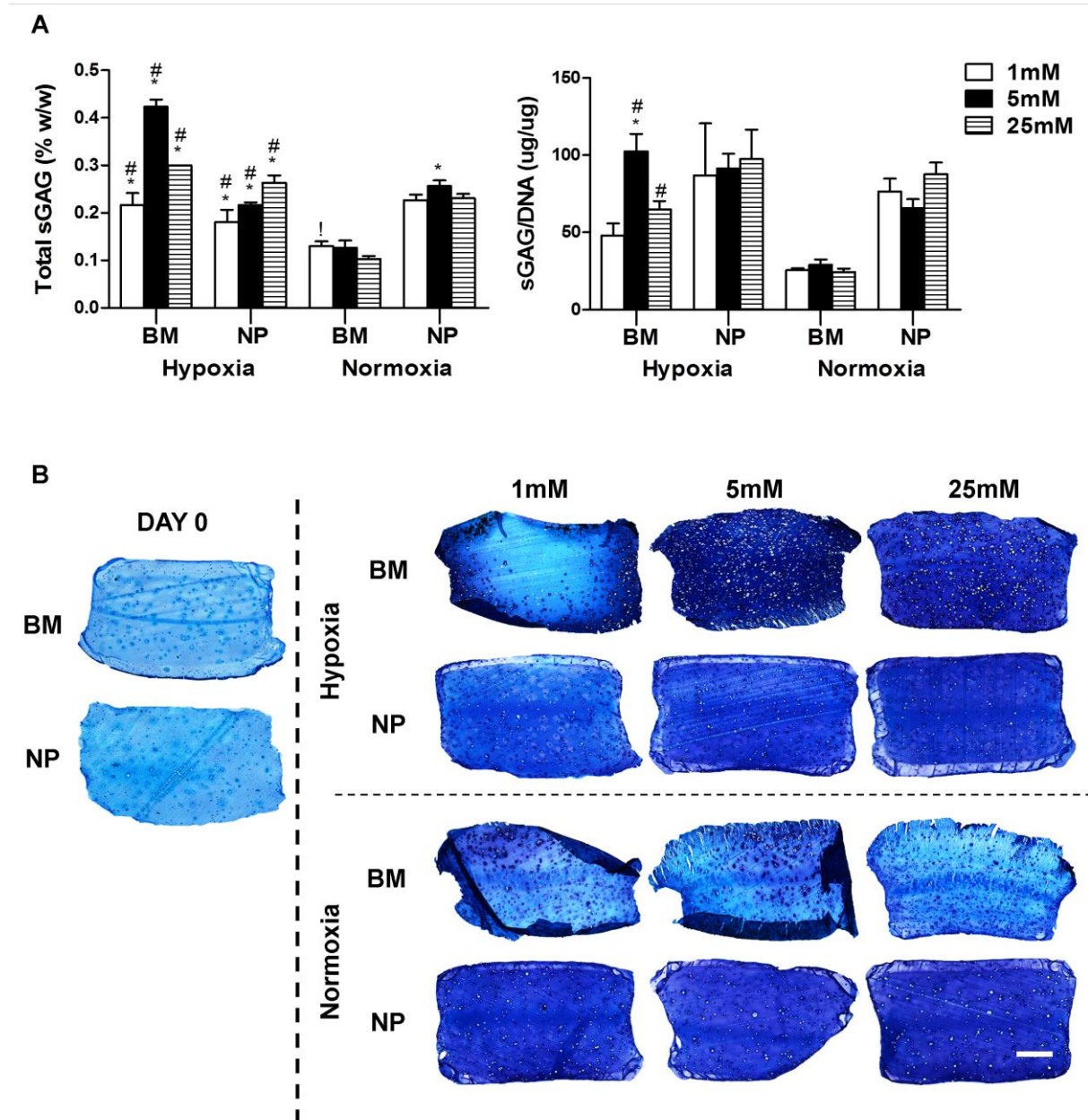
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399

Figure Legends

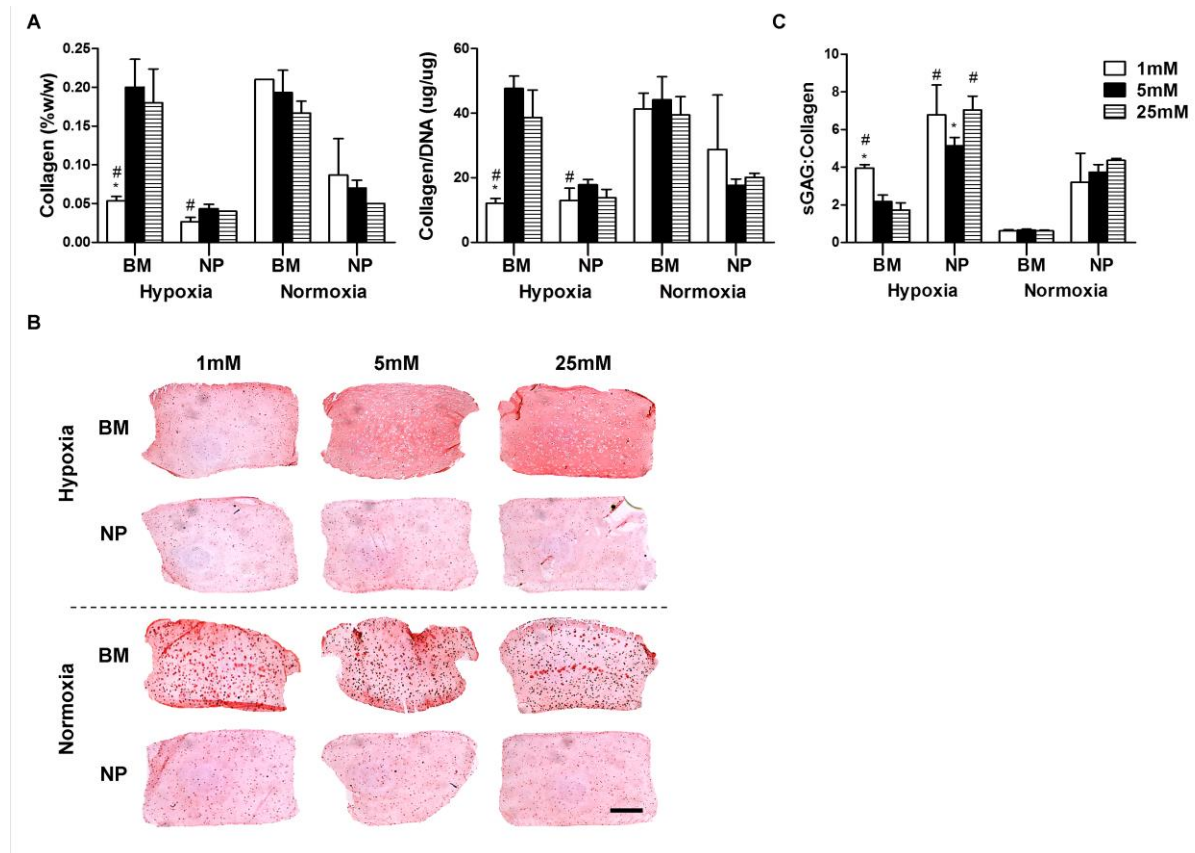


**Figure 1** (A) DNA content normalised to wet weight at day 21 for nucleus pulposus (NP) and bone marrow (BM) stem cells maintained under different glucose conditions (1mM, 5mM, 25mM) in hypoxia (5% O<sub>2</sub>) or normoxia (20% O<sub>2</sub>), # denotes significance compared to normoxia for same cell type, ! denotes significance compared to other glucose condition for same cell type (p<0.05); dashed line represents Day 0 DNA content (B) Cell viability for NP and BM constructs at Day 0 and Day 21. Scale bar =1mm.



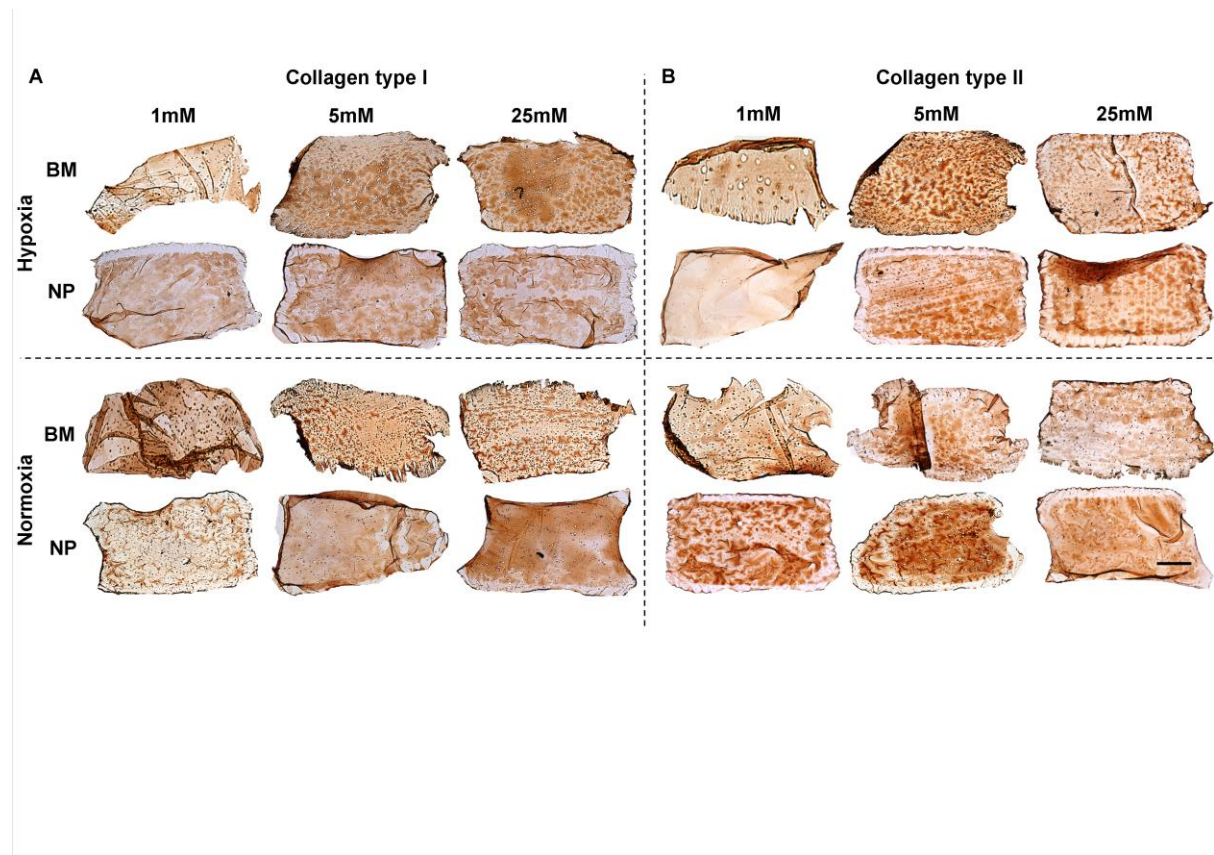
**Figure 2** (A) Total sGAG normalized to wet weight and to DNA content at day 21 for nucleus pulposus (NP) and bone marrow (BM) stem cells maintained under different glucose conditions (1mM, 5mM, 25mM) in hypoxia (5% O<sub>2</sub>) or normoxia (20% O<sub>2</sub>), # denotes significance compared to normoxia for same cell type, ! denotes significance compared to one other glucose condition for same cell type, \* denotes significance compared to both other glucose conditions for same cell type (p<0.05) (B) Histological evaluation with aldehyde fuchsin and alcian blue to identify sGAG at day 0 and day 21; deep blue/purple staining

indicates GAG accumulation and light blue staining indicates residual alginate. Scale bar = 1mm.



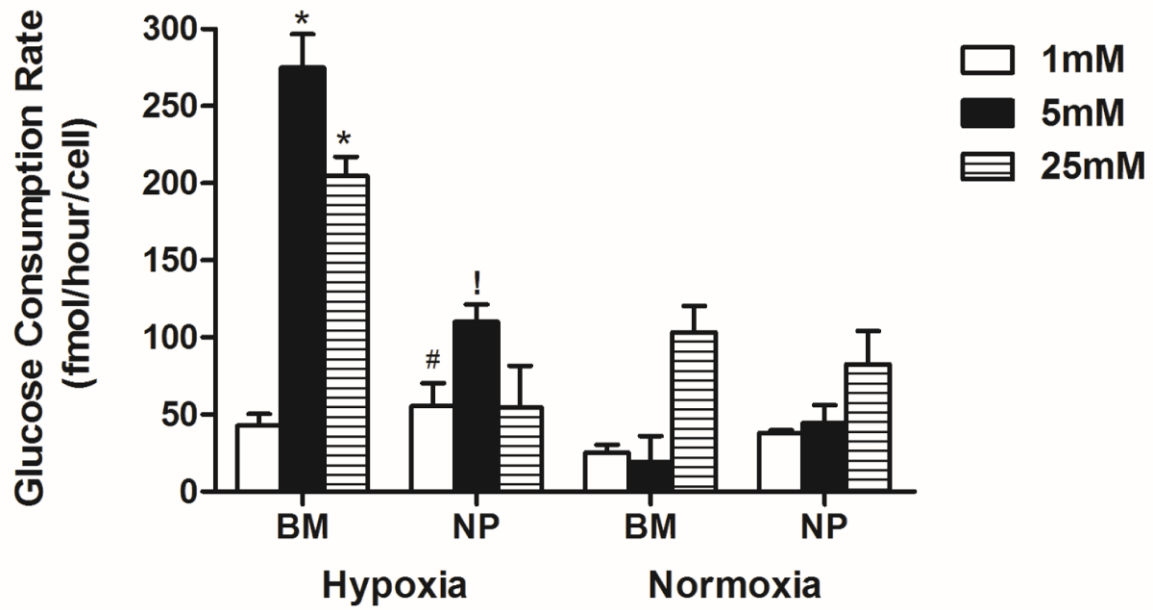
**Figure 3** (A) Total Collagen normalized to wet weight and to DNA at day 21 for nucleus pulposus (NP) and bone marrow (BM) stem cells maintained under different glucose conditions (1mM, 5mM, 25mM) in hypoxia (5% O<sub>2</sub>) or normoxia (20% O<sub>2</sub>), # denotes significance compared to normoxia for same cell type, \* denotes significance compared to both other glucose conditions for same cell type ( p<0.05) (B) Histological evaluation with picro-sirius red to identify collagen at day 21. Scale bar = 1mm. (C) sGAG:Collagen ratio at day 21; # denotes significance compared to normoxia for same cell type, \* denotes significance compared to both other glucose conditions for same cell type (p<0.05)

*Matrix Production by Nucleus Pulposus and Bone Marrow Stem Cells*



**Figure 4** Immunohistochemical evaluation at day 21 for (A) Collagen type I (B) Collagen type II for nucleus pulposus (NP) and bone marrow (BM) stem cells maintained under different glucose conditions (1mM, 5mM, 25mM) in hypoxia (5% O<sub>2</sub>) or normoxia (20% O<sub>2</sub>).

Scale bar = 1mm.



**Figure 5** Glucose consumption rate (fmol/hour/cell) at day 21 for nucleus pulposus (NP) and bone marrow (BM) stem cells maintained under different glucose conditions (1mM, 5mM, 25mM) in hypoxia (5% O<sub>2</sub>) or normoxia (20% O<sub>2</sub>), # denotes significance compared to normoxia for same cell type and glucose condition, \* denotes significance compared to all other groups for same glucose condition (p<0.05). ! denotes significance for NP in hypoxia compared to all other groups for same glucose condition.

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