

25 **Abstract**

26 Spray drying is a well-established scale-up technique for the production of cocrystals.
27 However, to the best of our knowledge, the effect of introducing a third component into the
28 feed solution during the spray drying process has never been investigated. Cocrystal
29 formation in the presence of a third component by a one-step spray drying process has the
30 potential to reduce the number of unit operations which are required to produce a final
31 pharmaceutical product (e.g. by eliminating blending with excipient). Sulfadimidine (SDM),
32 a poorly water soluble active pharmaceutical ingredient (API), and 4-aminosalicylic acid
33 (4ASA), a hydrophilic molecule, were used as model drug and coformer respectively to form
34 cocrystals by spray drying in the presence of a third component (excipient). The solubility of
35 the cocrystal in the excipient was measured using a thermal analysis approach. Trends in
36 measured solubility were in agreement with those determined by calculated Hansen
37 Solubility Parameter (HSP) values. The ratio of cocrystal components to excipient was
38 altered and cocrystal formation at different weight ratios was assessed. Cocrystal integrity
39 was preserved when the cocrystal components were immiscible with the excipient, based on
40 the difference in Hansen Solubility Parameters (HSP). For immiscible systems (difference in
41 $HSP > 9.6 \text{ MPa}^{0.5}$), cocrystal formation occurred even when the proportion of excipient was
42 high (90% w/w). When the excipient was partly miscible with the cocrystal components,
43 cocrystal formation was observed post spray drying, but crystalline API and coformer were
44 also recovered in the processed powder. An amorphous dispersion was formed when the
45 excipient was miscible with the cocrystal components even when the proportion of excipient
46 used as low (10% w/w excipient). For selected spray dried cocrystal-excipient systems an
47 improvement in tableting characteristics was observed, relative to equivalent physical
48 mixtures.

49

50

51 **Keywords**

52 Spray drying, cocrystals, sulfadimidine, 4-aminosalicylic acid, Hansen Solubility Parameter,
53 industrial production intensification

54

55

56

57

58 **1. Introduction**

59 It has been shown that the reason less than 1% of drug candidates make it to market is not
60 only due to a lack of efficacy, safety or an unfavourable side effect profile, but also due to
61 poor biopharmaceutical properties (Aakeröy Cb Fau - Aakeröy et al.; Cook et al., 2014). It
62 has been suggested that drug discovery strategies, such as high throughput screening, are
63 increasingly leading to lead candidates which have unfavourable physicochemical properties
64 (Lipinski et al., 2012). Many of these compounds have poor aqueous solubility, which can
65 lead to a low dissolution rate (Hörter and Dressman, 2001). Over half of marketed drug
66 products are formulated as salts to modify the physical properties of the active
67 pharmaceutical ingredient (API) . However, a major limitation of this approach is the
68 requirement of the API to possess a basic or acidic ionisable group. Pharmaceutical cocrystals
69 offer an alternative to salt forms as a means of improving the solubility, dissolution and
70 bioavailability of poorly water soluble drugs. Cocrystals of an API and coformer are formed
71 by noncovalent, freely reversible interactions, and so the presence of an ionisable group is not
72 a necessity. The solubility and dissolution rate of an API in a cocrystal are improved by
73 lowering the lattice energy and/or increasing the solvent affinity (Thakuria et al., 2013).
74 Cocrystallisation of an API can confer a number of advantages over other formulation
75 strategies such as amorphisation. One of the major limitations of amorphous forms is the fact
76 that they are thermodynamic unstable, making them prone to conversion to the lower energy
77 crystalline forms (Hancock et al., 1995).

78 Various methods exist to produce cocrystals. Common approaches include grinding and
79 solution methods. However, a disadvantage of solution methods to produce cocrystals can be
80 the formation of single component crystals when crystallised from an incongruently
81 saturating solution (Qiao et al., 2011). Spray drying is commonly used to produce amorphous
82 solid dispersions (Van den Mooter et al., 2001; Zhao et al., 2012) but also, in some instances,
83 results in the formation of crystalline materials (Kumar et al., 2015). This technique has been
84 shown to be a viable and scalable method to produce pure cocrystals from both congruent and
85 incongruently saturating solutions. Carbamazepine-glutaric acid, theophylline-nicotinamide,
86 urea-succinic acid and caffeine-glutaric acid all formed pure cocrystals when spray dried
87 from an incongruently saturating solutions. Further to this, the urea-succinic acid 1:1
88 cocrystal was discovered and consistently generated in pure form by spray drying.
89 Cocrystallisation of this system did not occur by slurry or reaction crystallisation methods
90 (Alhalaweh and Velaga, 2010).

91 The approach of using Hansen Solubility Parameters (HSP) calculated using the group
92 contribution method has enabled the prediction of solid-solid solubility of pharmaceutical
93 materials (Greenhalgh et al.; Hancock et al., 1997). For drug-excipient combinations, a $\Delta\delta t$
94 (i.e. difference in HSP) of less than $7.0 \text{ MPa}^{1/2}$ is considered to be indicative of significant
95 miscibility, while a $\Delta\delta t$ of greater than $10.0 \text{ MPa}^{1/2}$ denotes a lack of miscibility and limited
96 ability to form glass solutions (Forster et al., 2001; Greenhalgh et al.).

97 Calculation of the HSP of drug and coformer and the difference in HSP values for the two
98 components can be used as a tool to predict the success of cocrystal formation on spray
99 drying. It has been shown that, in order for an API to form a cocrystal with a coformer, the
100 two molecules must be miscible at a molecular level, with the difference in HSP being less
101 than $7 \text{ MPa}^{0.5}$ (Mohammad et al., 2011). However, to the best of our knowledge, the effect on
102 cocrystal formation of introducing a third (excipient) component into the feed solution during

103 the spray drying process has never been investigated, nor has the relative differences in HSP
104 between excipient and cocrystal components been probed in relation to success or otherwise
105 of cocrystal formation on spray drying.

106 The hypothesis underlying this work is that a larger difference in HSP between the cocrystal
107 components and the excipient will promote cocrystal formation during spray drying in the
108 presence of a carrier excipient, as the cocrystal components will not be miscible with the
109 excipient, and so will remain phase separated from the excipient but still interact with one
110 another. In contrast, excipients which have a similar HSP to the cocrystal components may be
111 miscible and may not allow for cocrystal formation to occur, rather there may be a high
112 probability that an amorphous dispersion of individual cofomer molecules, rather than a
113 cocrystal suspension would form within the carrier.

114 The aim of this work was to investigate the impact of including a carrier excipient on
115 cocrystal formation during the spray drying process. A range of pharmaceutical excipients
116 were selected and co-spray dried with the cocrystal components. Solid state characterisation
117 was performed as well as solubility studies of the cocrystal in the excipient using a thermal
118 analysis approach. Dissolution studies were performed from constant surface area disks.

119 The feasibility of co-spray drying cocrystals and a third component, carrier excipient, in order
120 to reduce the number of unit processes to produce a final pharmaceutical product was
121 investigated by compaction studies.

122

123

124 **2. Materials**

125 Sulfadimidine (SDM), 4-aminosalicylic acid (4ASA), mannitol, chitosan (average molecular
126 weight 50,000-190,000), glycine, polyvinyl alcohol (PVA) (average molecular weight
127 70,000-100,000), dextran (average molecular weight 68,800), hydroxypropyl methylcellulose
128 (HPMC) (4,000 cP) and polyvinylpyrrolidone K15 (PVP) were purchased from Sigma-
129 Aldrich (Ireland). Microcrystalline cellulose (MCC) Avicel[®] CL-611 was a gift from FMC
130 Biopolymer, Belgium. Soluplus[®] was a gift from BASF, Germany. Inulin with an average
131 degree of polymerisation of 11 (Fruitafit[®] HD) was a gift from Sensus, Netherlands. Ethanol
132 was supplied by Corcoran Chemicals (Ireland). Water was purified and filtered using an Elix
133 3 connected to a Synergy UV system (Millipore, UK). All other chemicals used were of
134 analytical grade.

135

136 **3. Methods**

137 **3.1. Preparation of cocrystals**

138 **Spray Drying**

139 A 1% w/v solution of SDM and 4-ASA was prepared using ethanol as solvent. The solution
140 was sonicated to dissolve the cocrystal components completely. An equal volume of 1% w/v
141 excipient aqueous solution (inulin, mannitol, glycine, PVA (heated to 60 °C), HPMC, PVP
142 and Soluplus) or suspension (MCC, chitosan and dextran) was added to the 1% solution of
143 SDM and 4-ASA. The solution with the cocrystal components was mixed with the excipient
144 solution/suspension prior to spray drying. The resultant solutions/suspensions were spray
145 dried using a Büchi B-290 Mini Spray Dryer operating in the open mode. The
146 solutions/suspensions were delivered to a 2-fluid atomization nozzle using a peristaltic pump
147 at a pump speed of 30 % (9-10 ml/min) and the aspirator was operated at 35 m³/hr. The

148 flowmeter for the standard 2-fluid nozzle was set at 4 cm, which is equivalent to 667
149 normlitrres per hour (Nl/h) of gas flow at standard temperature and pressure conditions
150 ($p=1013.25$ mbar and $T=273.15$ K) (Büchi Labortechnik, 93001). The inlet temperature was
151 set at 105 °C (outlet temperature between $68 - 72$ °C) for the systems which contained
152 excipient in deionised water and 78 °C (outlet temperature between $50 - 57$ °C) for the spray
153 drying of cocrystal in ethanol alone. Based on whether cocrystal formation occurred at this
154 ratio of cocrystal component to excipient (i.e. 1:1 %w/w), the ratio of cocrystal components
155 to excipient was altered to assess the maximum ratio of excipient:cocrystal components
156 which would allow cocrystal formation.

157 For comparison purposes, physical mixtures of cocrystal and excipients were prepared using
158 an agate mortar and pestle.

159 **Solvent Evaporation**

160 Equimolar proportions of SDM and 4ASA were dissolved in 60 ml of acetone to give a
161 0.01M solution and stirred until complete dissolution was achieved. The resulting solution
162 was placed in a fumehood and allowed to evaporate for 72 hours (Serrano et al., 2016a).

163

164 **3.2. Solid State Characterisation**

165 **Powder X-Ray Diffraction**

166 Powder X-ray analysis was performed using a Miniflex II Rigaku diffractometer with Ni-
167 filtered Cu $K\alpha$ radiation (1.54 Å). The tube voltage and tube current used were 30 kV and 15
168 mA, respectively. The PXRD patterns were recorded ($n=3$) for 2 theta ranging from 5° to 40°
169 at a step scan rate of 0.05° per second. Rigaku Peak Integral software was used to determine
170 peak intensity for each sample using the Sonneveld-Visser background edit procedure.

171 **Differential Scanning Calorimetry (DSC)**

172 DSC was performed using a Mettler Toledo DSC 821e instrument under nitrogen purge.
173 Powder samples (4-6 mg) were placed in aluminium pans (40 μ l), sealed, pierced to provide
174 three vent holes and heated at a rate of 10°C/min in the temperature range of 25 to 250 °C.
175 Temperature and enthalpy were calibrated using indium as standard. The DSC was controlled
176 by Mettler Toledo STARe software (version 6.10) working on a Windows NT operating
177 system. All reported temperatures refer to onset of melting.

178 **Solubility of Cocrystal in Excipient**

179 Physical mixtures of cocrystal and excipient were prepared by mixing in a pestle and mortar
180 at different weight ratios. The melting enthalpy of the crystalline phase was determined by
181 DSC (as described above) and plotted as a function of excipient weight fraction. The
182 solubility of the cocrystal in excipient was determined by extrapolating the linear plot of the
183 mass fraction against melting enthalpy to zero melting enthalpy, as previously described
184 (Amharar et al., 2014). Annealing was not performed due to the thermal instability of 4-ASA.

185 **Attenuated Total Reflectance Fourier Transform Infrared Spectroscopy (ATR-FTIR)**

186 Infrared spectra were recorded on a PerkinElmer Spectrum 1 FT-IR Spectrometer equipped
187 with a UATR and a ZnSe crystal accessory. Each spectrum was scanned in the range of 650-
188 4000 cm^{-1} with a resolution of 4 cm^{-1} . Data were evaluated using Spectrum v 5.0.1. software.
189 Four scans of each sample were taken.

190 **Scanning Electron Microscope (SEM)**

191 The surface images of the samples were captured at various magnifications by SEM using a
192 Zeiss Supra Variable Pressure Field Emission Scanning Electron Microscope (Germany)
193 equipped with a secondary electron detector at 5 kV. Samples were glued onto carbon tabs,

194 mounted on to aluminium pin stubs and sputter-coated with gold/palladium under vacuum
195 prior to analysis (Serrano et al., 2016b).

196 **3.3. Physical stability studies**

197 Spray dried samples (100 mg) were placed in glass vials and stored in conditions of 25 °C
198 and 60% relative humidity, with the required humidity provided by using a saturated solution
199 of sodium bromide. After seven days, samples were removed and analysed by PXRD.

200 **3.4. Intrinsic dissolution studies**

201 The intrinsic dissolution studies of solid materials were performed using a Woods intrinsic
202 dissolution apparatus (Elementec, Ireland). This allowed the dissolution to be measured from
203 constant surface area discs. Discs were prepared by compressing the powder (200 mg) into
204 compacts using a PerkinElmer hydraulic press with an 8 mm (diameter) punch and die set at a
205 pressure of 3 tonnes for a 1 min dwell time. The dissolution studies were carried out in
206 deionised water (volume: 900 mL, temperature: 37 °C) at a rotation speed of 100 rpm.
207 Aliquots (5 ml) were withdrawn with volume replacement at appropriate time intervals.
208 Samples were filtered through 0.45 µm filters and analysed for SDM and 4-ASA content by
209 HPLC. The study was performed in triplicate. The intrinsic dissolution rate (IDR) was
210 determined from the slope of the dissolution time profiles over the first 10 minutes. All
211 dissolution studies were carried out for samples with a 50% (w/w) ratio of excipient and
212 cocrystal. At the end of the experiments, the discs were recovered, dried at ambient
213 temperature and analysed by PXRD for process induced phase transformation.

214 Statistical analysis of dissolution profiles was performed using DDSolver (Zhang et al.,
215 2010). Univariate ANOVA analysis and Similarity Factor (f_2) analysis was performed to
216 compare drug dissolution profiles (Yuksel et al., 2000). An f_2 value between 50-100 indicates
217 that dissolution profiles are similar.

218 **3.5. High Performance Liquid Chromatography (HPLC)**

219 The concentration of SDM and 4-ASA in solution were determined as previously described
220 (18) using an Alliance HPLC with a Waters 2695 Separations module system and Waters
221 2996 photodiode array detector. The mobile phase consisted of methanol and phosphate
222 buffer pH 6.5 in 40:60 (v/v) ratio. The buffer was prepared from a 50 mM dipotassium
223 phosphate solution adjusted to pH 6.5 with phosphoric acid. The mobile phase was vacuum
224 filtered through a 0.45 µm membrane filter (Pall Supor[®] 0.45 µm, 47 mm) and bath sonicated
225 for 5 min. Separation was performed on a Phenomenex Inertsil ODS (3) C18 column (150
226 mm length, diameter 4.6 mm, particle size 5 µm) at a UV detection wavelength of 265 nm.
227 An injection volume of 20 µL was used. The elution was carried out isocratically at ambient
228 temperature with a flow rate of 1 mL/min. Elution times for 4-ASA and SDM were 1.9 min
229 and 4.0 min respectively. Empower software was used for peak evaluation (Grossjohann et
230 al., 2015).

231 **3.6. Compactability of cocrystals and cocrystal-polymer systems**

232 Tensile strength and ejection force of the co-spray dried systems and physical mixtures of
233 cocrystal with MCC (50:50 w/w) or cocrystal with inulin and MCC (60:20:20 w/w/w) were
234 investigated. Flat tablets (n=6, 100 mg) were compressed using a Natoli NP-RD10 (Saint
235 Charles, MO, USA) laboratory-scale single punch tablet press supplied with an Enerpac
236 (Menomonee Falls, WI, USA) P-392 manual pump with a RC-104 hydraulic cylinder
237 working in the range from 0 to 10 tonnes and standard 8-mm diameter punch and die tooling
238 (I Holland Limited, UK). Compaction properties were quantified in terms of hardness
239 achieved at the applied compaction pressure of 6 kN (0.612 tonnes). The pressure was
240 released immediately after the desired compression pressure was reached. Tablets were
241 pushed out of the die using the bottom punch and ejection force was recorded. A set of 6
242 tablets was subjected to radial hardness testing using a Dr Schleuniger, Pharmatron model 6D

243 tablet tester (Thun, Switzerland) (Serrano et al., 2016a). Tensile strength was calculated as
244 indicated in Equation 1:

$$245 \quad \sigma = \frac{2 * F}{\pi * D * H} \quad (\text{Eq. 1})$$

246 in which σ is the tensile strength, F is the radial hardness, D is the tablet diameter, and H is
247 the tablet thickness. After compaction, it was monitored whether or not the tablet capped
248 under the applied pressure and if the breakage of the tablet occurred in a consistent manner.
249 The PXRD pattern of the formulation before and after compaction was compared.

250 3.7. Hansen Solubility Parameter Calculation

251 Hansen solubility parameters were calculated from the chemical structures using the Van
252 Krevelen method (Van Krevelen and Te Nijenhuis, 2009). The weight average molecular
253 weights were used to determine solubility parameters for polymeric excipients (Scott, 1992).
254 The total HSP contribution was divided into three partial solubility parameters: dispersion
255 (δ_d), polar (δ_p) and hydrogen bonding (δ_h). The total solubility parameter was calculated as
256 indicated in Equations 2-5:

$$257 \quad \delta_t = (\delta_d^2 + \delta_p^2 + \delta_h^2)^{0.5} \quad (\text{Eq. 2})$$

$$258 \quad \delta_d = \frac{\sum_{i=1}^n F_{di}}{\sum_{i=1}^n v_i} \quad (\text{Eq. 3})$$

$$259 \quad \delta_p = \frac{(\sum_{i=1}^n F_{pi}^2)^{0.5}}{\sum_{i=1}^n v_i} \quad (\text{Eq. 4})$$

$$260 \quad \delta_h = \left(\frac{\sum_{i=1}^n F_{hi}}{\sum_{i=1}^n v_i} \right)^{0.5} \quad (\text{Eq. 5})$$

261

262 where i is the structural group within the molecule, F_{di} is the group contribution of the
263 dispersion forces, F_{pi} is the group contribution of the polar forces, F_{hi} is the group
264 contribution of the hydrogen bonding forces, and V_i is the group contribution of the molar
265 volume (Mohammad et al., 2011).

266 **4. Results**

267 **4.1. Effect of the type and composition of excipient on cocrystal formation by** 268 **spray drying**

269 **SDM/4-ASA cocrystal:excipient 50:50 (w/w)**

270 The polymorph II of the SDM:4-ASA cocrystal, the crystal structure of which has previously
271 been determined by single crystal XRD (Grossjohann et al., 2015), was generated by spray
272 drying. The X-ray diffraction pattern of SDM:4-ASA cocrystal and individual components
273 are depicted in Figure 1, as well as the cocrystal prepared by slow solvent evaporation from
274 acetone. DSC analysis of the cocrystals produced by solvent evaporation and spray drying
275 showed a single endothermic peak, characteristic of cocrystal melting. The cocrystal
276 produced by solvent evaporation had a higher melting point ($175.84 \pm 0.85^\circ\text{C}$) and a melting
277 enthalpy ($239.15 \pm 6.84 \text{ J/g}$) compared to that produced by spray drying, which had a melting
278 point of $170.08 \pm 0.23^\circ\text{C}$ and a melting enthalpy of $216.52 \pm 3.69 \text{ J/g}$. This is in agreement
279 with previously reported data (Grossjohann et al., 2015). This finding can be explained by the
280 fact that rapid drying processes such as spray drying are likely to induce crystal lattice
281 imperfections such as point defects, line defects and plane defects, which can affect the
282 thermal properties of the spray dried product (Corrigan, 1995).

283 PXRD demonstrated cocrystal formation was preserved when cocrystal components were
284 spray dried in the presence of inulin, MCC, dextran and mannitol at a 50% (w/w) ratio of

285 cocrystal components to 50% (w/w) of excipient. PXRD analyses showed that the same
286 diffraction peaks were present when compared to the spray dried cocrystal. Characteristic
287 diffractions peaks of the cocrystal are observed at 11.9° , 13.65° , 20.25° and 24.4° 2θ (Serrano
288 et al., 2016a). It would be expected that cocrystal formation would occur in the presence of a
289 suspended excipient (which was the case for MCC, chitosan and dextran), as the cocrystal
290 components in solution would be phase separated from the excipient in suspension. Extra
291 diffraction peaks were present for the cocrystal in mannitol system which were attributed to
292 mannitol (both alpha and delta polymorphs). Characteristic peaks of delta mannitol are
293 present at 9.75° and 25.2° 2θ , while characteristic alpha mannitol peaks are observed at 17.3°
294 and 33.2° 2θ . Spray drying of mannitol and lysosome has previously been shown to produce
295 a system containing a mixture of mannitol polymorphs, and both beta and delta polymorphs
296 of mannitol were observed (Hulse et al., 2009). However, the intensity of the diffraction
297 peaks was decreased for the co-spray dried cocrystal in excipient system when compared to a
298 physical mixture of the spray dried cocrystal and excipient, probably due to the interaction
299 between the cocrystal components and the excipient, and partial amorphisation of cocrystal
300 within the excipient matrix. Reduction in peak intensity may also be attributed to crystal
301 imperfections and/or the preferred orientation effect (Grant and York, 1986). The observed
302 decrease in intensity varied for each excipient used. PXRD analyses of of physical mixtures
303 of cocrystal and excipient are shown in Figure S1, Supplementary material.

304 The melting enthalpy associated with the co-spray dried cocrystal in inulin system was 91.81
305 ± 2.62 J/g, compared with a value of 98.7 ± 5.45 J/g for a physical mixture of the spray dried
306 cocrystal and inulin. The co-spray dried dextran in cocrystal system showed an enthalpy of
307 99.11 ± 5.4 J/g, compared to a value of 103.21 ± 9.13 J/g for the physical mixture of dextran
308 and spray dried cocrystal. The excipient which showed the largest difference in enthalpy
309 between the co-spray dried system and the physical mixture was MCC, with values of 83.52

310 ± 4.23 J/g and 101.02 ± 9.59 J/g respectively. In all cases, the only endothermic event was
311 attributed to the melting of the cocrystal, and no exothermic events were observed. It was not
312 possible to accurately measure the enthalpy of melting for the cocrystal when mannitol was
313 used as an excipient. Mannitol melted at $165.46 \pm 0.47^\circ\text{C}$, which overlapped with the melting
314 of the cocrystal. Based on the DSC analyses, the relative crystallinities of the co-spray dried
315 systems compared to the physical mixtures were 93.02%, 96.03% and 82.68% for the
316 systems containing inulin, dextran and MCC respectively. The co-spray dried systems had a
317 similar melting temperature as the physical mixture of cocrystal and excipient for all systems
318 with the exception of MCC, where a significant melting point depression was seen for the co-
319 spray dried formulation when compared to the physical mixture. DSC analyses of the
320 physical mixtures are shown in Figure S2, Supplemental material.

321 Bragg diffraction peaks attributable to the cocrystal, as well as the individual components
322 (API and coformer), were observed when cocrystal components were spray dried in the
323 presence of PVA, glycine and chitosan at a 50:50 %w/w ratio. Characteristic diffraction
324 peaks of glycine were also present in that particular system (Figure S3, Supplementary
325 material). An amorphous solid dispersion was produced when cocrystal components were
326 spray dried in the presence of Soluplus, HPMC and PVP at the 50/50% (w/w) ratio (Figure
327 S4, Supplementary material).

328 Based on the calculated HSP, inulin, MCC, mannitol, chitosan and dextran are immiscible
329 with the cocrystal components with a difference in HSP between the excipient and cocrystal
330 ranging from $9.6 \text{ MPa}^{0.5} - 18.6 \text{ MPa}^{0.5}$ (Table 1). All of these spray dried systems, with the
331 exception of chitosan, resulted in the formation of a cocrystal and there was no evidence of
332 other (individual API or coformer) components present by PXRD. Characteristic diffraction
333 peaks of the cocrystal and SDM were observed for the spray dried system containing

334 chitosan. As chitosan is a basic polymer, there may be an interaction with the acidic
335 coformer, resulting in the presence of Bragg peaks attributed to “free” SDM.

336 The differences in HSP between PVA and glycine and the cocrystal are $4.9 \text{ MPa}^{0.5}$ and 6.6
337 $\text{MPa}^{0.5}$, respectively which can explain the presence of diffraction peaks of both the cocrystal
338 and the individual components, due to the partial miscibility of the cocrystal components
339 within these excipients. It may be hypothesised that the interaction of the excipient with the
340 cocrystal components can result in the formation of an amorphous dispersion. The diffraction
341 peaks observed may be as a result of the rapid crystallisation of a binary, ternary or single
342 component amorphous domains. The crystallisation of materials by spray drying is thought to
343 be a two stage process, with material transforming from the liquid to an amorphous phase
344 first, and then from the amorphous phase to a crystalline phase (Chiou and Langrish, 2008)
345 The differences in HSP between PVP, Soluplus and HPMC were even lower ($4.4 \text{ MPa}^{0.5}$, 3.9
346 $\text{MPa}^{0.5}$ and $1.9 \text{ MPa}^{0.5}$ respectively). Spray drying led to the formation of an amorphous solid
347 dispersion instead of a cocrystal (Figure S3, Supplemental material) probably due to the
348 higher miscibility of the cocrystal components in these excipients.

349

350 **4.2. Effect of different ratios of excipient on cocrystal formation during spray drying**

351 **PVP, Soluplus and HPMC**

352 The ratio of cocrystal components to excipient was altered to assess whether the HSP
353 difference reflected the ratio at which a cocrystal would form when co-spray dried with an
354 excipient. PVP, Soluplus and HPMC were chosen and different cocrystal:excipient weight
355 ratios (75:25, 80:20, 90:10) investigated.

356 At the lowest ratio of excipient (10% w/w), the cocrystal was formed when PVP and Soluplus
357 were the excipients used. However, an amorphous dispersion was formed in the case of

358 HPMC (data not shown). It has previously been determined that viscous polymers can inhibit
359 the crystallisation process. The fast evaporation of solvent which occurs during the drying
360 process can lead to a rapid viscosity increase and permit kinetic trapping of the cocrystal
361 components in the excipient matrix as an amorphous form or disordered system (Paudel et al.,
362 2013). As the HPMC solution has a higher viscosity than the PVP and Soluplus solutions
363 (data not shown), both the higher viscosity and the lower difference in HSP between the
364 cocrystal components and HPMC may contribute to the formation of an amorphous
365 dispersion.

366 For PVP and Soluplus, cocrystal formation was observed when excipients were co-spray
367 dried at a ratio of 80:20 (w/w) cocrystal components to excipient (Figure 2i, iii). When the
368 ratio was altered to 75:25 (w/w) cocrystal components to excipient, an amorphous dispersion
369 was formed in the case of both excipients. The three co-spray dried PVP and Soluplus
370 systems at different ratios were then stressed under conditions of 25°C and 60% relative
371 humidity (RH) for one week. An increased intensity of the Bragg peaks was observed in
372 those co-spray dried systems containing 80% and 90% cocrystal. Co-spray dried cocrystal
373 components and PVP at a 75% (w/w) cocrystal components to 25% (w/w) ratio crystallised
374 from an amorphous dispersion to the metastable polymorph II cocrystal (Grossjohann et al.,
375 2015) under these conditions. Peaks attributable to individual components or to the form I
376 cocrystal (22) were not observed. In contrast, when the 75:25 (w/w) cocrystal
377 components:Soluplus system was stressed, diffraction peaks attributable to both the form II
378 and more stable form I cocrystal were present (Figure 2ii, iv). When the cocrystal alone
379 (which presents as form II) was stressed under the same conditions, a polymorphic transition
380 to the form I cocrystal was not observed, suggesting that stressing co-spray dried cocrystal:
381 Soluplus (75:25% w:w) from the amorphous state results in a metastable form II.

382

383 **Chitosan**

384 Diffraction peaks attributable to both the cocrystal and individual components were seen
385 when chitosan (50% w/w) was co-spray dried with cocrystal components (50% w/w). This
386 ratio was altered to determine the maximum ratio at which cocrystal formation will occur
387 without the presence of individual components. Cocrystal formation occurred when 10%,
388 20% and 25% (w/w) chitosan was co-spray dried with the cocrystal components. When 30%
389 of chitosan was used, cocrystal as well as the peaks of individual components were observed,
390 probably due to the interaction between the chitosan and the 4ASA, as previously
391 commented. DSC thermograms showed that the melting temperature of the co-spray dried
392 system with chitosan varied between 164 to 167°C (Figure 3) .

393

394 **MCC**

395 A cocrystal was formed in the presence of MCC when the cocrystal components (50% w/w)
396 were co-spray dried with MCC (50% w/w). As a cocrystal formed at this ratio, the amount of
397 MCC relative to cocrystal components was increased to assess the maximum ratio at which
398 cocrystal formation would occur. Cocrystal formation was observed up to a 30:70,
399 cocrystal:MCC weight ratio. A reduction in intensity of Bragg peaks attributable to the
400 cocrystal was seen when the ratio of MCC to cocrystal components was increased (Figure 4i).
401 The diffraction pattern was devoid of characteristic Bragg peaks of the individual
402 components. The melting point depression of the cocrystal with increasing MCC composition
403 suggests the formation of a more imperfect crystalline form of the cocrystal when higher
404 ratios of MCC are used. A broader melting peak can be attributed to imperfect crystalline
405 form (Figure 4iii). After stressing at 25°C and 60% RH for seven days, characteristic Bragg

406 peaks of the cocrystal were observed even at the lowest ratio (cocrystal: MCC, 20:80) (Figure
407 4ii).

408

409 **4.3. Morphology**

410 Spray drying resulted in cocrystal microspheres between 1-10 μm (Figure 5). Microparticle
411 surface and morphology was dependent on the excipient used, but also on the excipient-
412 cocrystal ratio. In those systems where the cocrystal was formed, microspheres exhibited
413 rough surfaces with embedded crystals at the surface (Figure 5a-d) whereas, in those systems
414 where an amorphous solid dispersion was formed, microspheres exhibited smooth surfaces
415 (for example with PVP at 50%). When the ratio of PVP was reduced to 10%, cocrystal
416 formation occurred and microspheres with rough surfaces were observed (Figure 5f).

417

418 **4.4. ATR-FTIR**

419 The H-bonding interaction between the cocrystal and the excipients were analysed by ATR-
420 FTIR (Figure 6). Distinctive bands in the higher frequency range were observed for the single
421 components. Asymmetric and symmetric stretching bands of $-\text{NH}_2$ of 4ASA were observed at
422 3493 cm^{-1} and 3386 cm^{-1} . SDM displays asymmetric and symmetric stretching bands of the
423 NH_2 group at 3441 cm^{-1} and 3339 cm^{-1} respectively. The sulphonamide NH group shows a
424 stretching band at 3235 cm^{-1} . The molecular interaction through hydrogen bond formation
425 between SDM and 4ASA spray dried cocrystal was characterised by: i) two broad bands, one
426 at 3482 cm^{-1} and one at 3372 cm^{-1} with a shoulder attributable to the N-H stretching of the
427 NH_2 amine group of 4ASA which were shifted towards lower wavenumbers from 3493 cm^{-1}
428 and 3386 cm^{-1} and ii) sulfone ($-\text{SO}_2$) stretching in SDM and $-\text{OH}$ deformation in 4ASA at
429 1315 cm^{-1} and 1275 cm^{-1} , respectively (Grossjohann et al., 2015). The same bands were seen

430 for both the spray dried cocrystal alone and the co-spray dried systems (containing inulin,
431 mannitol, MCC and dextran), indicating no interaction between the cocrystal and the
432 excipient during spray drying. Hydrogen bonding attributable to cocrystal formation is not
433 seen when PVP and Soluplus were co-spray dried with the cocrystal components at the 50:50
434 %w/w ratio. In Figure 5, the co-spray dried system with inulin is illustrated. Co-spray dried
435 systems with dextran, MCC, mannitol, PVP and Soluplus at the 50% (w/w) ratio are
436 presented in Figure S5-S9, supplementary material).

437

438 **4.5. Solubility of cocrystal in excipient**

439 We hypothesised that cocrystal formation occurs in the presence of an excipient when the
440 single components are not miscible with the excipient, as determined by the difference in
441 HSP between the components and excipient. In order to correlate the difference in HSP with
442 the miscibility of the cocrystal with the excipient matrix, the solubility of the spray dried
443 cocrystal and the individual cocrystal components in the amorphous excipients (inulin, MCC,
444 dextran, chitosan, PVA, PVP, Soluplus and HPMC) was determined by the zero melting
445 enthalpy extrapolation method (Amharar et al., 2014). The solubility of the cocrystal in
446 inulin, MCC and dextran was 3.69% w/w, 3.85% w/w and 3.83% w/w, respectively, which
447 was relatively low (Figure 7). These results were in agreement with the differences in HSP
448 between the cocrystal and excipient of $18.6 \text{ MPa}^{0.5}$, $12.5 \text{ MPa}^{0.5}$ and $9.6 \text{ MPa}^{0.5}$ respectively,
449 indicating that the formation of the cocrystal at higher excipient ratios is likely to happen.
450 The solubility of cocrystal in chitosan was determined to be 3.23%. This value is in
451 agreement with the calculated HSP difference of $11.2 \text{ MPa}^{0.5}$ between the cocrystal and
452 chitosan (Figure 7). However, a cocrystal only formed at low ratios of chitosan possibly due
453 to the interaction between basic chitosan and acidic 4ASA.

454 The solubility of the cocrystal in PVA was 13.74 %w/w (Figure 8) and the difference in HSP
455 between the cocrystal and PVA was 4.9 MPa^{0.5}. Cocrystal solubility in PVP, Soluplus and
456 HPMC was much higher, 24.43%w/w, 25.21% w/w and 18.77 %w/w respectively (Figure 8).
457 These values were also in agreement with the differences in HSP between the cocrystal and
458 excipient, indicating higher miscibility between the cocrystal and the excipient justifying why
459 cocrystal formation only occurred when a low ratio of excipient was used. Similar solubility
460 values between the single components and the excipients were observed (Values in Table 2)
461 (Figure S10 – S12, Supplementary material).

462 **4.6. Dissolution Studies**

463 Dissolution of SDM and 4-ASA from the cocrystal started incongruently over the first 10 min
464 and became congruent subsequently (Figure S13, Supplementary material). During spray
465 drying, 4ASA can partially sublime, resulting in a mass loss of 4ASA, as previously reported
466 (Grossjohann et al., 2015). HPLC analysis of the spray dried cocrystal showed 3.5% less
467 molar amount of 4ASA in the final spray dried formulation. This resulted in an excess of
468 SDM in the spray dried product which can transform to the amorphous state upon spray
469 drying (Caron et al., 2011). Once the excess amorphous SDM crystallised, dissolution
470 became congruent.

471 No statistically significant differences in the f_2 value were found among the dissolution
472 profiles of the co-spray dried systems (50:50% w/w ratio) with inulin, mannitol or dextran
473 (Figure 9). Dissolution from a constant surface area could not be tested when MCC was used
474 as an excipient since, due to the disintegrant properties of MCC, the disk quickly
475 disintegrated. No differences were found between the intrinsic dissolution rates of the three
476 co-spray dried systems (Table 3). Therefore, it was concluded that the excipient used had no
477 impact on the dissolution of the cocrystal from the co-spray dried system.

478 After dissolution, the compacts were dried and analysed by PXRD for surface changes. A
479 polymorphic transformation from the form II to form I was observed from the co-spray dried
480 system with mannitol. In contrast, no polymorphic transformation was seen when dissolution
481 studies were performed with inulin and dextran (Figures S14 – S16, Supplementary material).
482 The compacts were smooth and homogenous before dissolution. After dissolution, the surface
483 was observed to be pitted due to the different dissolution rates of the excipient and cocrystal.

484

485 **4.7. Compactability of spray dried cocrystal:excipient systems**

486 As a proof of concept, the feasibility of co-spray dried systems to reduce the number of unit
487 processes to produce a final pharmaceutical product was investigated by compaction studies.
488 As MCC is commonly used as a tablet filler due to its excellent compression properties
489 (David and Augsburger, 1977), the compactability of the co-spray dried system with MCC
490 (50% w/w) and its corresponding physical mixture were assessed. Including more than one
491 excipient in the feed solution/suspension may allow for a blending step to be omitted, going
492 directly from a spray drying process to a direct compression. For this reason, the compaction
493 properties of a co-spray dried system containing 60 %w/w cocrystal, 20 %w/w inulin and 20
494 %w/w MCC was also assessed, along with a physical mixture with identical composition. It
495 has previously been reported that the SDM:4ASA cocrystal produced by spray drying is less
496 prone to capping than the cocrystal produced by solvent evaporation (Serrano et al., 2016a).
497 For the MCC systems, both the co-spray dried system and physical mixture produced tablets
498 with similar tensile strengths. A significant difference in ejection force was observed
499 however, with the co-spray dried system requiring a 5-fold lower force to eject the tablets
500 (Figure 10). No capped tablets were observed for both the co-spray dried system and the
501 physical mixture. PXRD analyses was performed to assess possible alteration of the crystal
502 structure during the tableting process. While an increase in Bragg peak intensity was

503 observed for the co-spray dried system after compaction, no deformation induced phase
504 transformation changes were observed (Figure S17, Supplementary material). For the system
505 containing both MCC and inulin, the co-spray dried system showed no tendency to capping
506 during compaction. Two capped tablets were observed for the physical mixture. These two
507 tablets were not tested further. Two extra tablets were made and tested. No differences were
508 observed in tensile strength between the co-spray dried system and the physical mixtures.
509 However, a significantly lower ejection force (19-fold) was observed for the co-spray dried
510 system (Figure 10), suggesting that the compaction properties of the co-spray dried system
511 were notably improved, due to less sticking characteristics. Possible alteration of the
512 cocrystal structure was evaluated by PXRD analysis before and after the compaction. No
513 deformation induced phase transformation changes were observed (Figure S18,
514 Supplementary material).

515

516 **5. Discussion**

517 This study has demonstrated the feasibility of cocrystal formation and inclusion within an
518 excipient matrix, through the process of co-spray drying. PXRD and DSC analysis for the
519 cocrystal-in-excipient systems were consistent with those of the cocrystal produced by
520 solvent evaporation, indicating that cocrystal formation still occurred when the cocrystal was
521 co-spray dried with some of the excipients included in this study.

522 Differences in DSC results were noted between the cocrystal-in-excipient systems and the
523 corresponding physical mixtures; it was found that the heat of fusion was lowered (and the
524 melting temperature depressed when higher ratios of excipient were used) for the co-spray
525 dried systems. PXRD results also revealed a loss of crystallinity, indicating that the spray

526 drying process induced some level of amorphisation of the cocrystal, without fully impeding
527 cocrystal formation.

528 Previously, it has been determined that a difference in HSP of less than 7 MPa^{0.5} indicates
529 that materials are miscible. This theory has been utilised to predict cocrystal formation,
530 whereby drug and coformer with $\Delta\text{HSP} < 7 \text{ MPa}^{0.5}$ were shown to be likely to form a
531 cocrystal due to their miscibility. In this study, the same principle was applied to predict
532 cocrystal formation in the presence of a carrier excipient. However, in this case it was
533 anticipated that the closer the value of HSP for the cocrystal and carrier excipient, the less
534 likely cocrystal formation would be because the carrier excipient would be miscible in the
535 cocrystal and thus prevent cocrystal formation. The findings from the study showed that a
536 clear correlation exists between the HSP difference between the cocrystal and carrier
537 excipient and the likelihood of cocrystal formation occurring. It can be deduced that $\Delta\text{HSP} >$
538 $9.6 \text{ MPa}^{0.5}$ for the cocrystal and carrier excipient leads to formation of the cocrystal when it is
539 co-spray dried with the carrier excipient. $\Delta\text{HSP} < 9.6 \text{ MPa}^{0.5}$ for the cocrystal and carrier
540 excipient results in either a completely amorphous form following co-spray drying, or
541 cocrystal with traces of the individual components (API, coformer) of the cocrystal.

542 The ratio of excipient:cocrystal had a major impact on cocrystal formation as well as the
543 overall miscibility between the cocrystal and the excipient. In order to get a deeper insight
544 into the process, a parameter to predict cocrystal formation (CFP) was calculated using
545 Equation 6:

546
$$CFP = \frac{\Delta\text{HSP}}{F_e + S} \quad (\text{Eq. 6})$$

547 Where ΔHSP is the difference in HSP between the cocrystal and the excipient, F_e is the
548 excipient fraction and S is the measured solubility of the cocrystal within the excipient
549 matrix. Based on the CFP calculated values and the experimental results (Table 4), it can be

550 concluded that for those systems with a CFP value > 10 , there is a high probability of
551 cocrystal formation, while values below 1 indicate that there is a high probability of co-
552 amorphous systems forming. Some exceptions were found, such as chitosan, probably due to
553 its basic behaviour and interaction in solution with the coformer decreasing the H-bonding
554 with SDM.

555 For those co-spray dried systems that allowed cocrystal formation, FTIR revealed no
556 interaction between the cocrystal and the excipient. Also, intrinsic dissolution studies showed
557 no differences in the SDM release rate among the different excipients suggesting that the
558 release of SDM was determined by the cocrystal itself. Preliminary studies on process
559 intensification showed that co-spray dried systems had better compaction properties than
560 physical mixtures, suggesting that a secondary excipient blending step might be avoided.

561 **6. Conclusions**

562 This work demonstrates that the introduction of a third component into the feed
563 solution/suspension prior to spray drying can result in a cocrystal embedded in excipient
564 matrix. Cocrystal formation can also occur when more than one excipient is added to the
565 spray drying feed solution/suspension. The difference in HSP between the cocrystal
566 components and the excipient can be used as a general parameter to predict if cocrystal
567 formation will occur. However, as was seen when the cocrystal components were co-spray
568 dried with chitosan, other factors such as the acidic/basic nature of the excipient can
569 influence whether cocrystal formation can occur. The difference in HSP can also be used to
570 predict the ratio at which a cocrystal can form when co-spray dried with an excipient. Co-
571 spray drying an excipient with the cocrystal components can result in cocrystal formation,
572 regardless of the crystalline or amorphous nature of the excipient. As spray drying is a
573 scalable unit operation used in the pharmaceutical industry, co-spray drying with an excipient

574 can reduce the number of unit operations required to produce a final pharmaceutical product,
575 as a separate blending step of the cocrystal and excipient could be avoided.

576

577 **Acknowledges**

578 This publication has emanated from research supported in part by a research grant from
579 Science Foundation Ireland (SFI) [Grant Number 12/RC/2275] and is co-funded under the
580 European Regional Development Fund.

581

582 **References**

583

- 584 (a) Handbook of Pharmaceutical Salts: Properties, Selection and Use; Stahl, P. H.; Wermuth, C. G.
585 Eds.; Verlag Helvetica Chimica Acta: Zu`rich,2002.(b)Bighley,L.D.;Berge,S.M.;Monkhouse,D.C. Salt
586 forms of drugs and absorption. In Encyclopedia of Pharmaceutical Technology; Swarbick, J.; Boylan,
587 J. C. Eds; Marcel Dekker, Inc.: New York, 1996; Vol. 13, pp 453-499. (c) Gu, C. H.; Grant, D. J. W.
588 Handbook of Experimental Pharmacology: Stereochemical Aspects of Drug Action and Disposition;
589 Eichelbaum, M.; Testa, B.; Somogyi, A. Eds.; Springer: Berlin, 2003.
- 590 Aakeröy Cb Fau - Aakeröy, C.B., Forbes S Fau - Forbes, S., Desper J Fau - Desper, J., Using Cocrystals
591 To Systematically Modulate Aqueous Solubility and Melting Behavior of an Anticancer Drug.
592 Alhalaweh, A., Velaga, S.P., 2010. Formation of Cocrystals from Stoichiometric Solutions of
593 Incongruently Saturating Systems by Spray Drying. *Crystal Growth & Design* 10, 3302-3305.
- 594 Amharar, Y., Curtin, V., Gallagher, K.H., Healy, A.M., 2014. Solubility of crystalline organic
595 compounds in high and low molecular weight amorphous matrices above and below the glass
596 transition by zero enthalpy extrapolation. *International Journal of Pharmaceutics* 472, 241-247.
- 597 Antoniou, E., Themistou, E., Sarkar, B., Tsianou, M., Alexandridis, P., 2010. Structure and dynamics of
598 dextran in binary mixtures of a good and a bad solvent. *Colloid and Polymer Science* 288, 1301-1312.
- 599 Caron, V., Tajber, L., Corrigan, O.I., Healy, A.M., 2011. A Comparison of Spray Drying and Milling in
600 the Production of Amorphous Dispersions of Sulfathiazole/Polyvinylpyrrolidone and
601 Sulfadimidine/Polyvinylpyrrolidone. *Molecular Pharmaceutics* 8, 532-542.
- 602 Chiou, D., Langrish, T.A.G., 2008. A comparison of crystallisation approaches in spray drying. *Journal*
603 *of Food Engineering* 88, 177-185.
- 604 Cook, D., Brown, D., Alexander, R., March, R., Morgan, P., Satterthwaite, G., Pangalos, M.N., 2014.
605 Lessons learned from the fate of AstraZeneca's drug pipeline: a five-dimensional framework. *Nat Rev*
606 *Drug Discov* 13, 419-431.
- 607 Corrigan, O.I., 1995. Thermal analysis of spray dried products. *Thermochimica Acta* 248, 245-258.
- 608 David, S.T., Augsburger, L.L., 1977. Plastic flow during compression of directly compressible fillers
609 and its effect on tablet strength. *Journal of pharmaceutical sciences* 66, 155-159.
- 610 Forster, A., Hemenstall, J., Tucker, I., Rades, T., 2001. Selection of excipients for melt extrusion with
611 two poorly water-soluble drugs by solubility parameter calculation and thermal analysis.
612 *International Journal of Pharmaceutics* 226, 147-161.

613 Grant, D.J.W., York, P., 1986. Entropy of processing: a new quantity for comparing the solid state
614 disorder of pharmaceutical materials. *International Journal of Pharmaceutics* 30, 161-180.

615 Greenhalgh, D.J., Williams, A.C., Timmins, P., York, P., Solubility parameters as predictors of
616 miscibility in solid dispersions. *Journal of Pharmaceutical Sciences* 88, 1182-1190.

617 Grossjohann, C., Serrano, D.R., Paluch, K.J., O'Connell, P., Vella-Zarb, L., Manesiotis, P., McCabe, T.,
618 Tajber, L., Corrigan, O.I., Healy, A.M., 2015. Polymorphism in Sulfadimidine/4-Aminosalicylic Acid
619 Cocrystals: Solid-State Characterization and Physicochemical Properties. *Journal of Pharmaceutical
620 Sciences* 104, 1385-1398.

621 Hancock, B.C., Shamblin, S.L., Zografi, G., 1995. Molecular mobility of amorphous pharmaceutical
622 solids below their glass transition temperatures. *Pharmaceutical research* 12, 799-806.

623 Hancock, B.C., York, P., Rowe, R.C., 1997. The use of solubility parameters in pharmaceutical dosage
624 form design. *International Journal of Pharmaceutics* 148, 1-21.

625 Hörter, D., Dressman, J.B., 2001. Influence of physicochemical properties on dissolution of drugs in
626 the gastrointestinal tract. *Advanced Drug Delivery Reviews* 46, 75-87.

627 Hulse, W.L., Forbes, R.T., Bonner, M.C., Getrost, M., 2009. Influence of protein on mannitol
628 polymorphic form produced during co-spray drying. *International Journal of Pharmaceutics* 382, 67-
629 72.

630 Kumar, S., Shen, J., Zolnik, B., Sadrieh, N., Burgess, D.J., 2015. Optimization and dissolution
631 performance of spray-dried naproxen nano-crystals. *International Journal of Pharmaceutics* 486,
632 159-166.

633 Lipinski, C.A., Lombardo, F., Dominy, B.W., Feeney, P.J., 2012. Experimental and computational
634 approaches to estimate solubility and permeability in drug discovery and development settings.
635 *Advanced drug delivery reviews* 64, 4-17.

636 Mohammad, M.A., Alhalaweh, A., Velaga, S.P., 2011. Hansen solubility parameter as a tool to predict
637 cocrystal formation. *International Journal of Pharmaceutics* 407, 63-71.

638 Paudel, A., Worku, Z.A., Meeus, J., Guns, S., Van den Mooter, G., 2013. Manufacturing of solid
639 dispersions of poorly water soluble drugs by spray drying: Formulation and process considerations.
640 *International Journal of Pharmaceutics* 453, 253-284.

641 Qiao, N., Li, M., Schlindwein, W., Malek, N., Davies, A., Trappitt, G., 2011. Pharmaceutical cocrystals:
642 An overview. *International Journal of Pharmaceutics* 419, 1-11.

643 Ravindra, R., Krovvidi, K.R., Khan, A.A., 1998. Solubility parameter of chitin and chitosan.
644 *Carbohydrate Polymers* 36, 121-127.

645 Rowe, R.C., 1988. Interaction of lubricants with microcrystalline cellulose and anhydrous lactose — a
646 solubility parameter approach. *International Journal of Pharmaceutics* 41, 223-226.

647 Scott, G., 1992. Properties of polymers. Their correlation with chemical structure; their numerical
648 estimation and prediction from additive group contributions. *Endeavour* 16, 97-98.

649 Serrano, D.R., O'Connell, P., Paluch, K.J., Walsh, D., Healy, A.M., 2016a. Cocrystal habit engineering
650 to improve drug dissolution and alter derived powder properties. *J Pharm Pharmacol* 68, 665-677.

651 Serrano, D.R., Persoons, T., D'Arcy, D.M., Galiana, C., Dea-Ayuela, M.A., Healy, A.M., 2016b.
652 Modelling and shadowgraph imaging of cocrystal dissolution and assessment of in vitro antimicrobial
653 activity for sulfadimidine/4-aminosalicylic acid cocrystals. *Eur J Pharm Sci* 89, 125-136.

654 Thakuria, R., Delori, A., Jones, W., Lipert, M.P., Roy, L., Rodríguez-Hornedo, N., 2013. Pharmaceutical
655 cocrystals and poorly soluble drugs. *International Journal of Pharmaceutics* 453, 101-125.

656 Van den Mooter, G., Wuyts, M., Bleton, N., Busson, R., Grobet, P., Augustijns, P., Kinget, R., 2001.
657 Physical stabilisation of amorphous ketoconazole in solid dispersions with polyvinylpyrrolidone K25.
658 *European Journal of Pharmaceutical Sciences* 12, 261-269.

659 Van Krevelen, D.W., Te Nijenhuis, K., 2009. Chapter 7 - Cohesive Properties and Solubility, Properties
660 of Polymers (Fourth Edition). Elsevier, Amsterdam, pp. 189-227.

661 Yuksel, N., Kanik, A.E., Baykara, T., 2000. Comparison of in vitro dissolution profiles by ANOVA-based,
662 model-dependent and -independent methods. *International Journal of Pharmaceutics* 209, 57-67.

663 Zhang, Y., Huo, M., Zhou, J., Zou, A., Li, W., Yao, C., Xie, S., 2010. DDSolver: An Add-In Program for
664 Modeling and Comparison of Drug Dissolution Profiles. *The AAPS Journal* 12, 263-271.
665 Zhao, M., Barker, S.A., Belton, P.S., McGregor, C., Craig, D.Q.M., 2012. Development of fully
666 amorphous dispersions of a low Tg drug via co-spray drying with hydrophilic polymers. *European*
667 *Journal of Pharmaceutics and Biopharmaceutics* 82, 572-579.

668

669

670

671

672 **Table 1. Cocrystal formation in excipient matrix when spray dried at a ratio of 50:50**
 673 **(w/w) cocrystal components: excipient.** The calculated HSP of SDM:4ASA cocrystal was
 674 26.8 MPa^{0.5}. Key, CC, cocrystal.

Excipient	Crystalline or amorphous nature of the excipient	δ_t (MPa ^{0.5}) of excipient (Reference)	$\Delta\delta_t$ (MPa ^{0.5}) between excipient and Cocrystal	PXRD of co-spray dried systems
Inulin	Amorphous	45.4	18.6	CC
MCC	Amorphous	39.3 (Rowe, 1988)	12.5	CC
Mannitol	Crystalline	39.1 (Forster et al., 2001)	12.3	CC
Chitosan	Amorphous	38 (Ravindra et al., 1998)	11.2	CC+API+coformer
Dextran	Amorphous	36.4 (Antoniou et al., 2010)	9.6	CC
Glycine	Crystalline	33.4	6.6	CC+API+coformer
PVA	Amorphous	31.7 (Forster et al., 2001)	4.9	CC+API+coformer
HPMC	Amorphous	28.7	1.9	Amorphous
PVP	Amorphous	22.4 (Forster et al., 2001)	4.4	Amorphous
Soluplus	Amorphous	22.9	3.9	Amorphous

675

676

677

678 **Table 2. Solubility values of cocrystal and individual components in excipients and the**
 679 **associated difference in HSP.**

System	Solubility (%w/w)	Difference in HSP (MPa^{0.5})
Cocrystal in Inulin	3.69	18.6
Cocrystal in MCC	3.85	12.5
Cocrystal in Chitosan	3.23	11.2
Cocrystal in Dextran	3.83	9.6
Cocrystal in PVA	13.74	4.9
Cocrystal in PVP	24.43	4.4
Cocrystal in Soluplus	25.21	3.9
Cocrystal in HPMC	18.77	1.9
SDM in Inulin	2.85	19.2
4ASA in Inulin	4.14	16.8
4ASA in MCC	1.77	10.7
SDM in Chitosan	2.50	11.8
4ASA in Chitosan	9.41	9.4
SDM in Dextran	5.68	10.2
4ASA in Dextran	5.10	7.8
SDM in PVA	13.88	5.5
4ASA in PVA	11.77	3.1
SDM in Soluplus	15.93	3.3
4ASA in PVP	27.52	6.2

680

681

682 **Table 3. Intrinsic dissolution rates of SDM calculated over the first 10 min.**

System, 50:50, w:w ratio	Initial Dissolution Rate (mg/cm²/min)
Cocrystal in inulin system	0.0712 ± 0.0027
Cocrystal in mannitol system	0.0812 ± 0.0013
Cocrystal in dextran system	0.0764 ± 0.0150

683

684

685

686 **Table 4. Prediction of cocrystal formation based on calculated CFP values (from Eq. 6).**
687 Darker areas (CFP < 1) indicate that the formation of a co-amorphous system is likely, while
688 lighter areas (CFP>10) indicate that there is a high likelihood of cocrystal formation to occur
689 in the co-spray dried system.

Excipient	Ratio of Excipient								
	0.1	0.2	0.3	0.4	0.5	0.6	0.7	0.8	0.9
Inulin	50.1	25.1	16.7	12.5	10	8.4	7.2	6.3	5.6
MCC	30.5	15.3	10.2	8	6.1	5.1	4.4	3.8	3.4
Chitosan	34.4	17.2	11.5	8.6	6.9	5.7	4.9	4.3	3.8
Dextran	24.8	12.4	8.3	6.2	5	4.1	3.5	3.1	2.8
PVA	3.5	1.7	1.2	0.9	0.7	0.6	0.5	0.4	0.4
PVP	1.6	0.8	0.5	0.4	0.3	0.3	0.2	0.2	0.2
Soluplus	1.5	0.8	0.5	0.4	0.3	0.3	0.2	0.2	0.2
HPMC	1	0.5	0.3	0.2	0.2	0.2	0.1	0.1	0.1

690

691

Production of Cocrystals in an Excipient Matrix by Spray Drying

David Walsh^{a,b}, Dolores R. Serrano^{a,b}, Zelalem Ayenew Worku^{a,b}, Brid A. Norris^{a,b}, Anne Marie Healy^{a,b*}

^aSchool of Pharmacy and Pharmaceutical Sciences, Trinity College Dublin, Dublin 2, Ireland.

^bSSPC, Synthesis and Solid State Pharmaceutical Centre, Ireland.

*Corresponding author:

Tel.: +353 1 896 1444

E-mail address: healyam@tcd.ie (A.M. Healy)

Figure 1. PXRD patterns and DSC thermograms of cocrystals and co-spray dried systems. i) PXRD patterns a) Cocrystal produced by spray drying, b) Cocrystal produced by slow solvent evaporation from acetone, c) Unprocessed 4ASA, d) Unprocessed SDM. **ii) PXRD pattern of co-spray dried systems with excipient at 50% w/w ratio.** a) Cocrystal produced by spray drying, b) Cocrystal components co-spray dried with dextran, c) Cocrystal components co-spray dried with inulin, d) Cocrystal components co-spray dried with MCC, e) Cocrystal components co-spray dried with mannitol. **iii) DSC thermograms.** a) Unprocessed SDM, b) Unprocessed 4ASA, c) Cocrystal produced by spray drying, d) Cocrystal produced by solvent evaporation, e) Cocrystal components co-spray dried with inulin, f) Cocrystal components co-spray dried with mannitol, g) Cocrystal components co-spray dried with MCC, h) Cocrystal components co-spray dried with dextran.

Figure 2. PXRD patterns of co-spray dried systems with soluplus and PVP. i) Co-spray dried with Soluplus and ii) Co-spray dried with Soluplus after stressing at 25 °C and 60% RH for seven days. a) Spray dried cocrystal, b) Cocrystal:soluplus (75:25, w:w), c) Cocrystal:soluplus (80:20, w:w), d) Cocrystal:soluplus (90:10, w:w). iii) Co-spray dried with PVP and iv) Co-spray dried with PVP after stressing at 25°C and 60% RH for seven days, a) Spray dried cocrystal, b) Cocrystal:PVP (75:25, w:w), c) Cocrystal:PVP (80:20, w:w), d) Cocrystal:PVP (90:10, w:w).

Figure 3. DSC thermograms (i) and PXRD pattern (ii) of co-spray dried cocrystal with chitosan. Key: **i)** a) Spray dried cocrystal, b) Unprocessed SDM, c) Unprocessed 4ASA, d) Cocrystal:Chitosan (75:25, w:w), e) Cocrystal:Chitosan (80:20, w:w), f) Cocrystal Cocrystal:Chitosan (90:10, w:w). **ii)** a) Spray dried cocrystal, b) Cocrystal:Chitosan (70:30, w:w), c) Cocrystal:Chitosan (75:25, w:w), d) Cocrystal:Chitosan (80:20, w:w), e) Cocrystal:Chitosan (90:10, w:w).

Figure 4. PXRD patterns of co-spray dried systems with MCC before (i) and after stressing (ii) at 25°C and 60% RH for seven days. Key: a) Spray dried cocrystal, b) Cocrystal:MCC (50:50, w:w), c) Cocrystal:MCC (40:60, w:w), d) Cocrystal:MCC (30:70, w:w), e) Cocrystal:MCC (20:80, w:w), f) Unprocessed MCC. **iii) DSC thermograms of co-spray dried systems with MCC.** Key: a) Spray dried cocrystal, b) Cocrystal:MCC (50:50, w:w), c) Cocrystal:MCC (40:60, w:w), d) Cocrystal:MCC (30:70, w:w), e) Cocrystal:MCC (20:80, w:w).

Figure 5. SEM micrographs. Key: a) Spray dried cocrystal, b) Co-spray dried cocrystal with inulin (50:50, w:w), c) Co-spray dried cocrystal with mannitol (50:50, w:w), d) Co-spray dried cocrystal with MCC (50:50, w:w), e) Co-spray dried cocrystal with PVP (50:50, w:w), f) Co-spray dried cocrystal with PVP (90:10, w:w).

Figure 6. FTIR analyses of a) co-spray dried cocrystal in inulin (50:50, w/w ratio), b) spray dried cocrystal, c) inulin, d) a physical mixture of SDM and 4ASA (1:1 molar ratio).

Figure 7. The solubility of the cocrystal in inulin (i), MCC (ii), chitosan (iii) and dextran (iv).

Figure 8. The solubility of the cocrystal in PVA (i), Soluplus (ii), HPMC (iii) and PVP (iv).

Figure 9. The release of SDM for the systems co-spray dried with inulin (black ■), mannitol (red ●) and dextran (blue ▲) with a 50:50% w/w ratio of excipient and cocrystal.

Figure 10. Tensile strength (circles) and ejection force (triangles) of i) co-spray dried system and physical mixtures of cocrystal 50%, MCC 50%, and ii) co-spray dried system and physical mixtures of cocrystal 60%, inulin 20% and MCC 20%, compacted at 6KN.

Figure 1

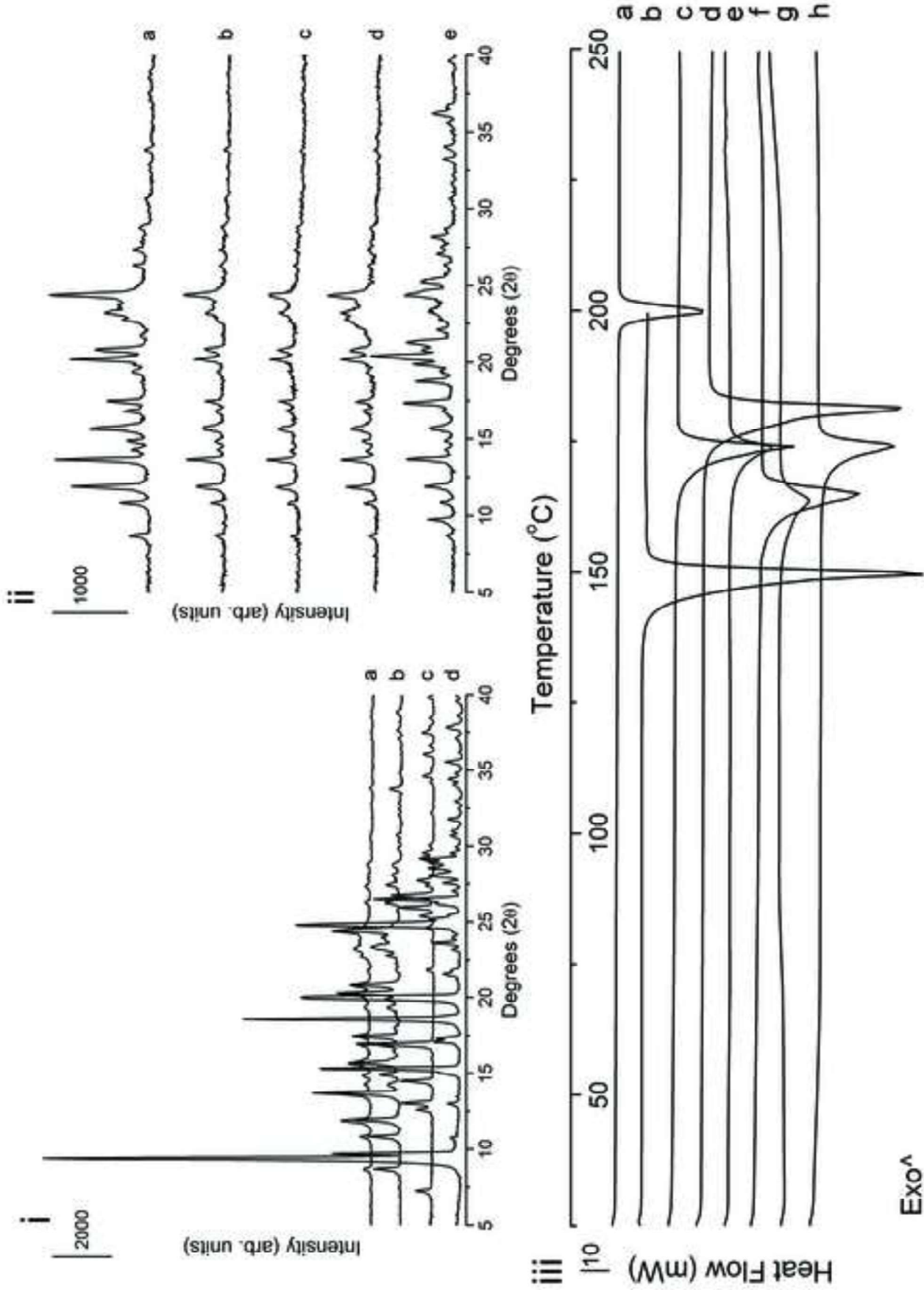


Figure 2

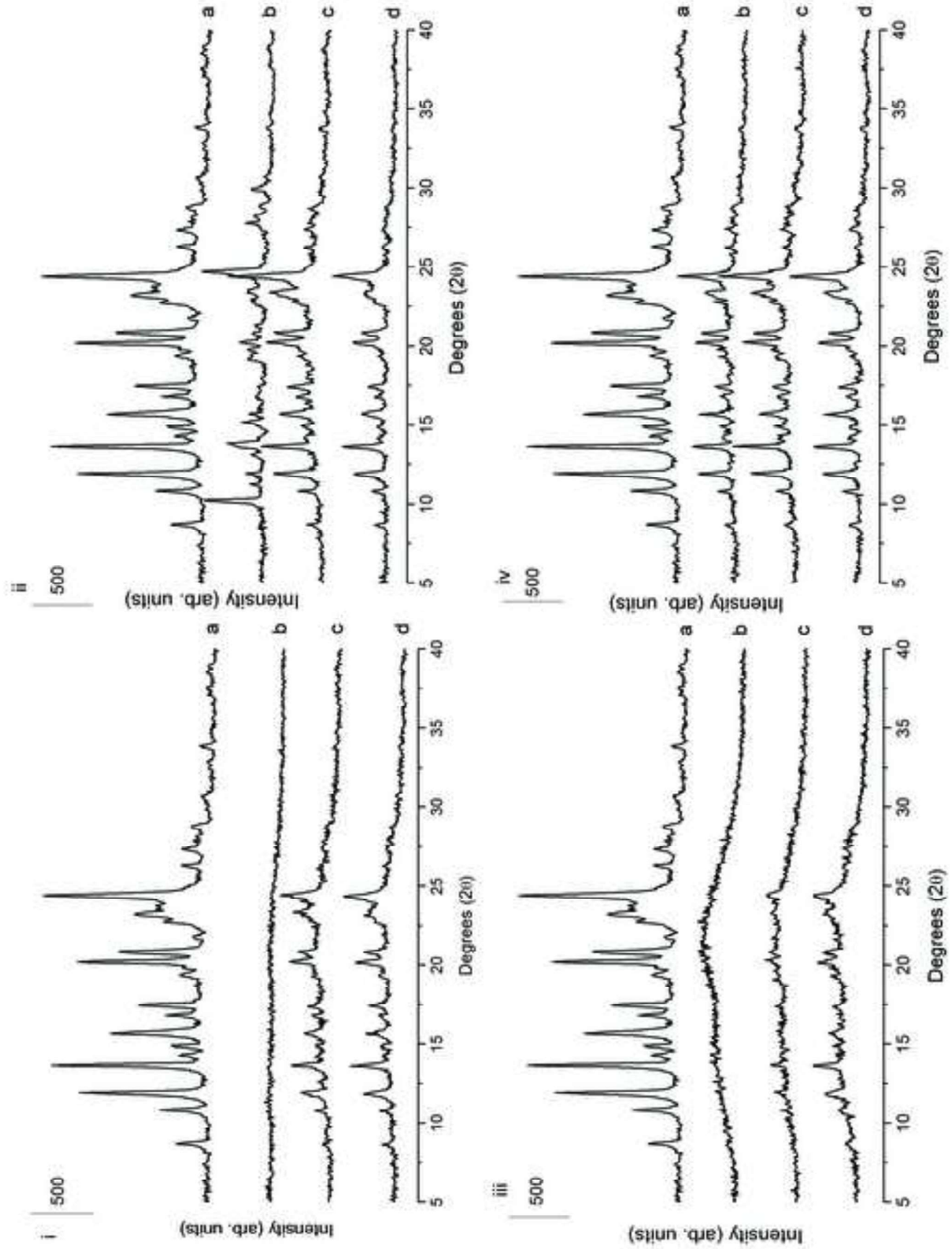


Figure 3

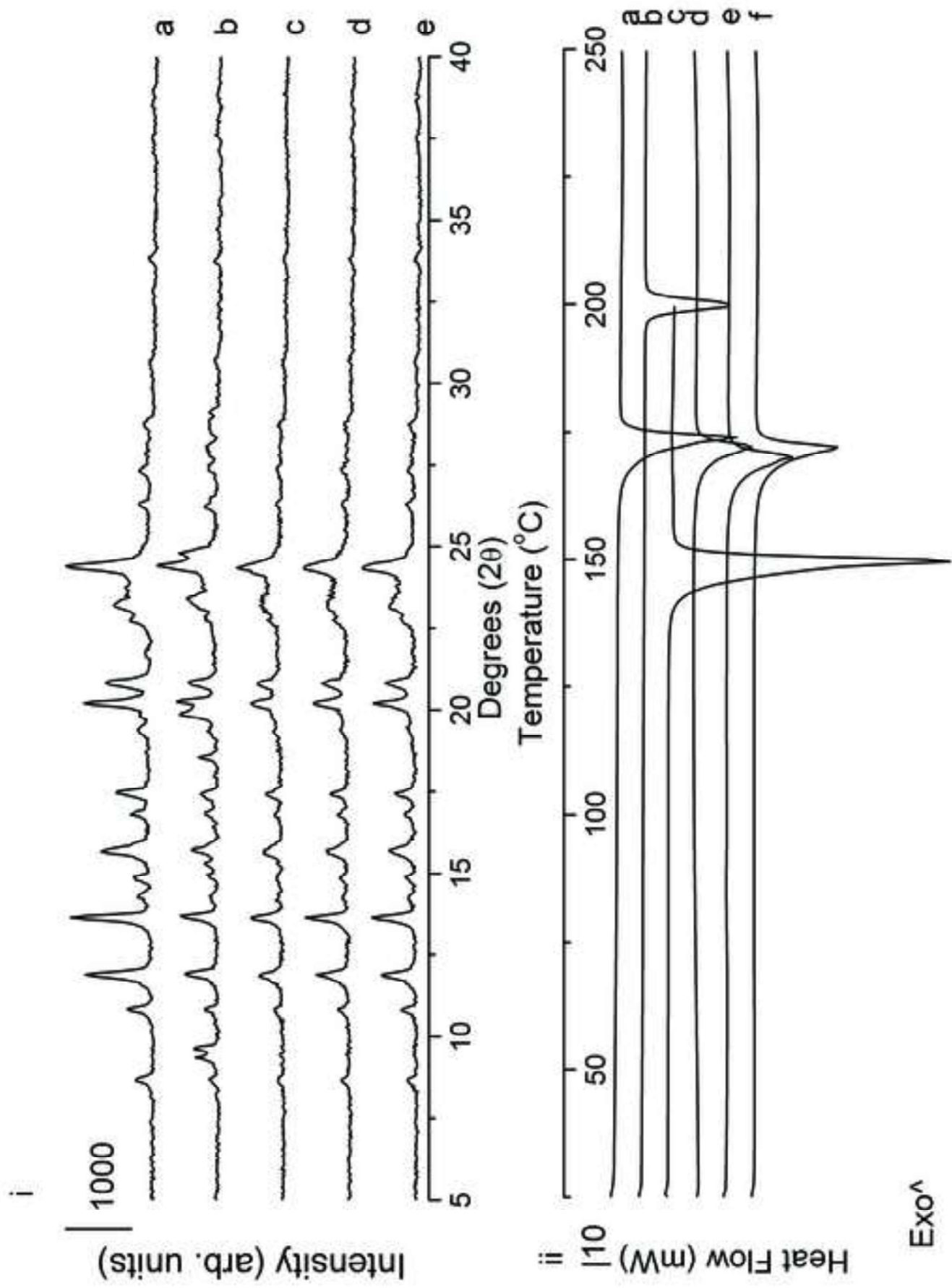


Figure 4

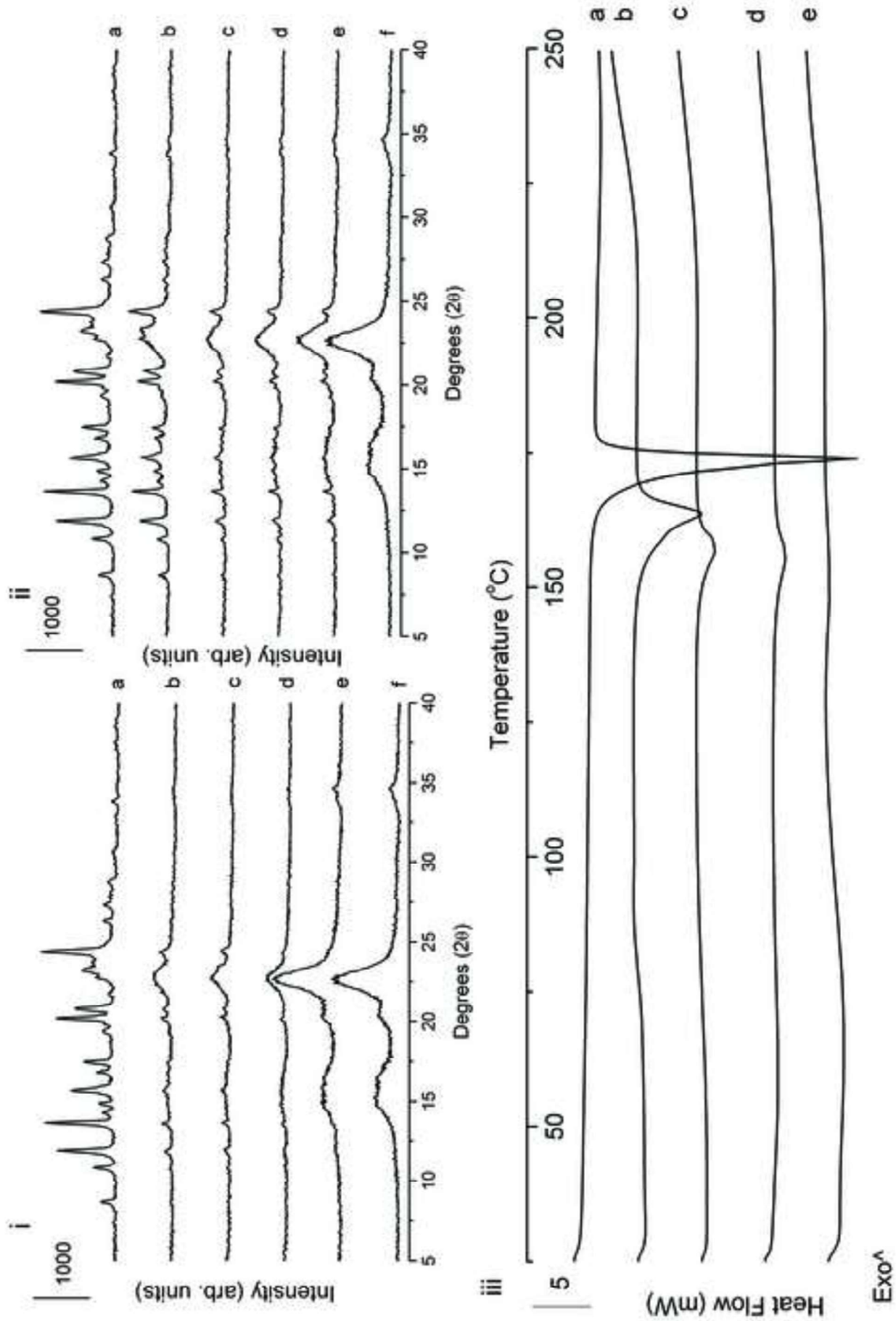


Figure 5

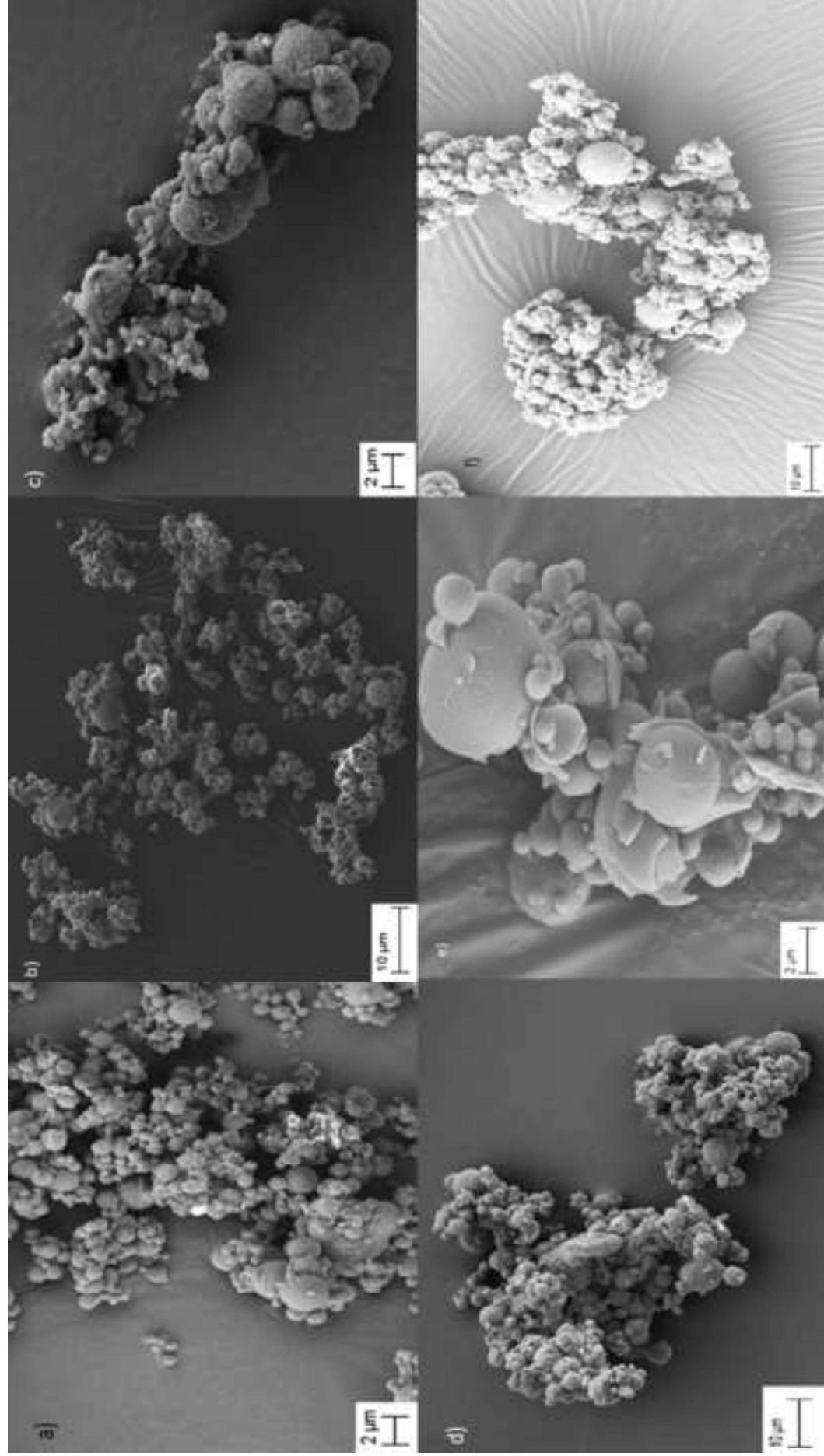


Figure 6

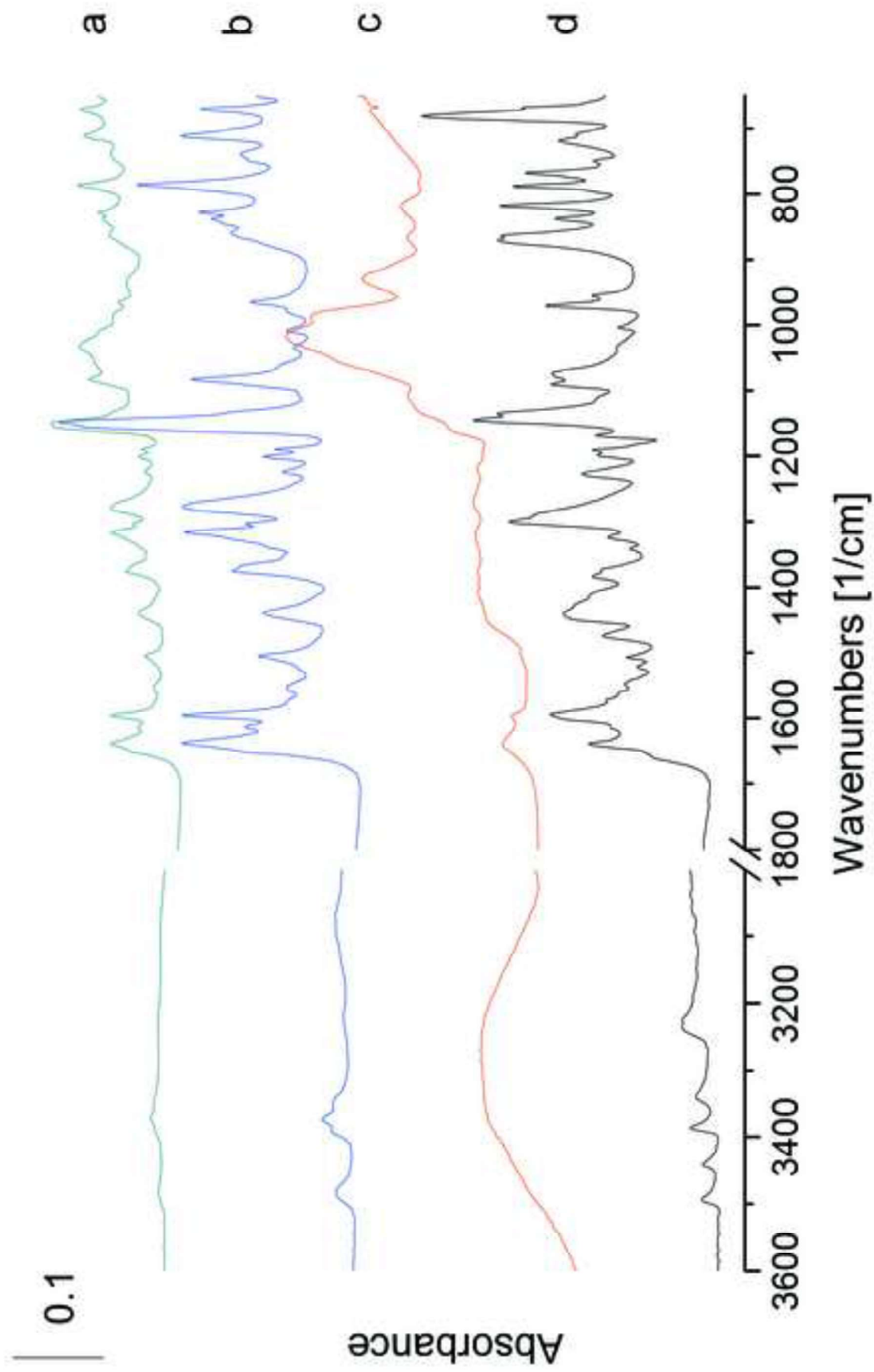


Figure 7

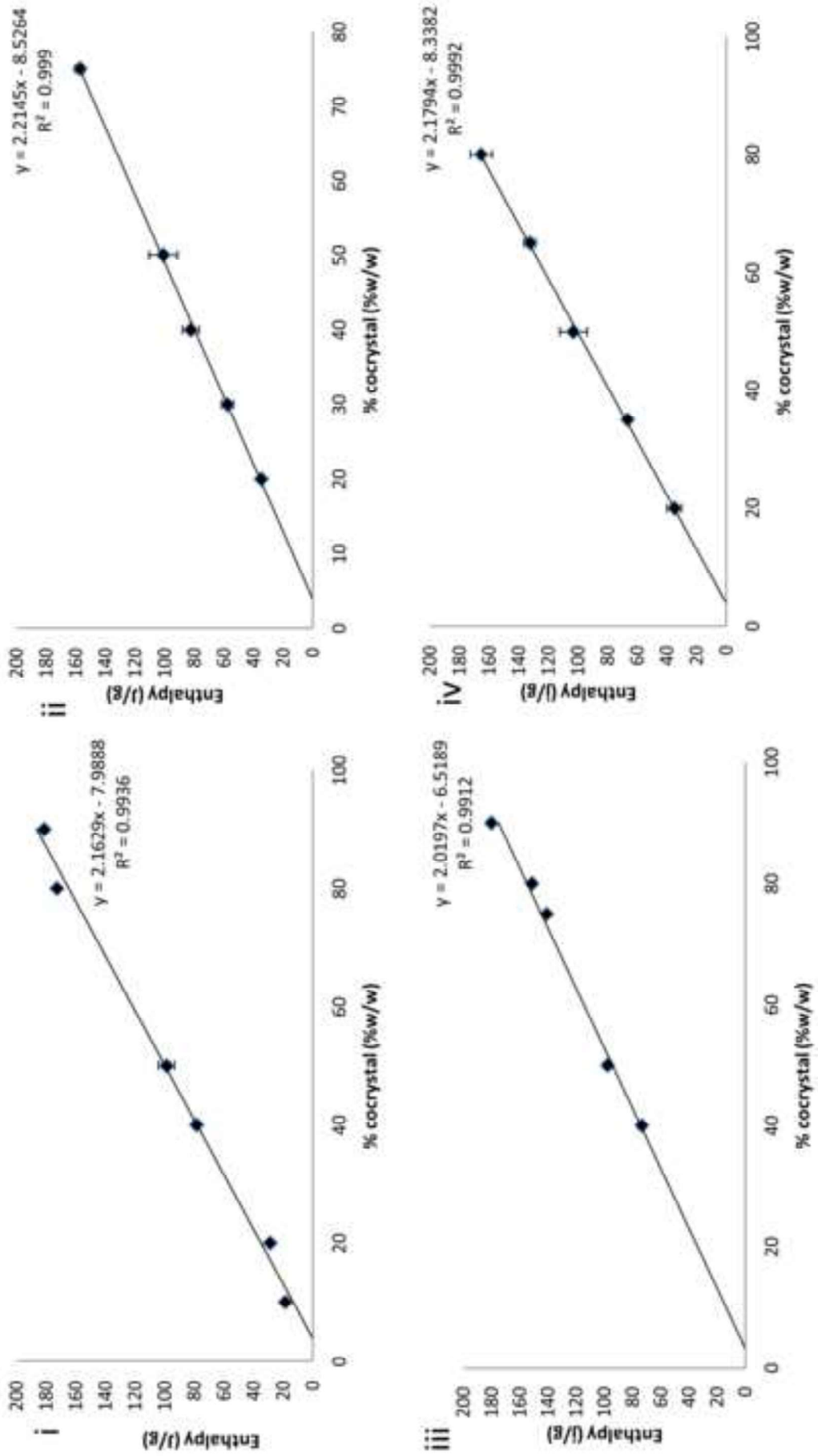
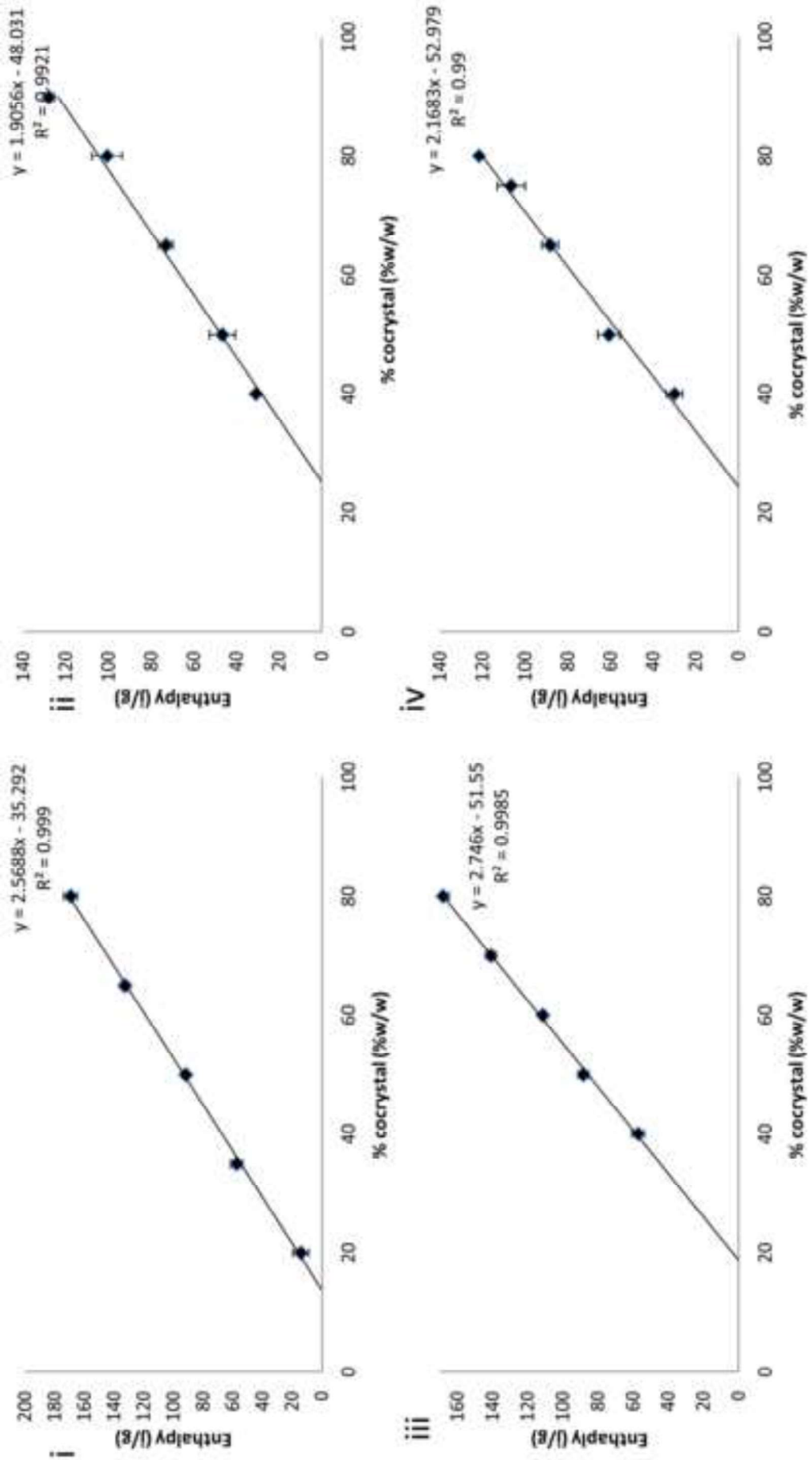


Figure 8



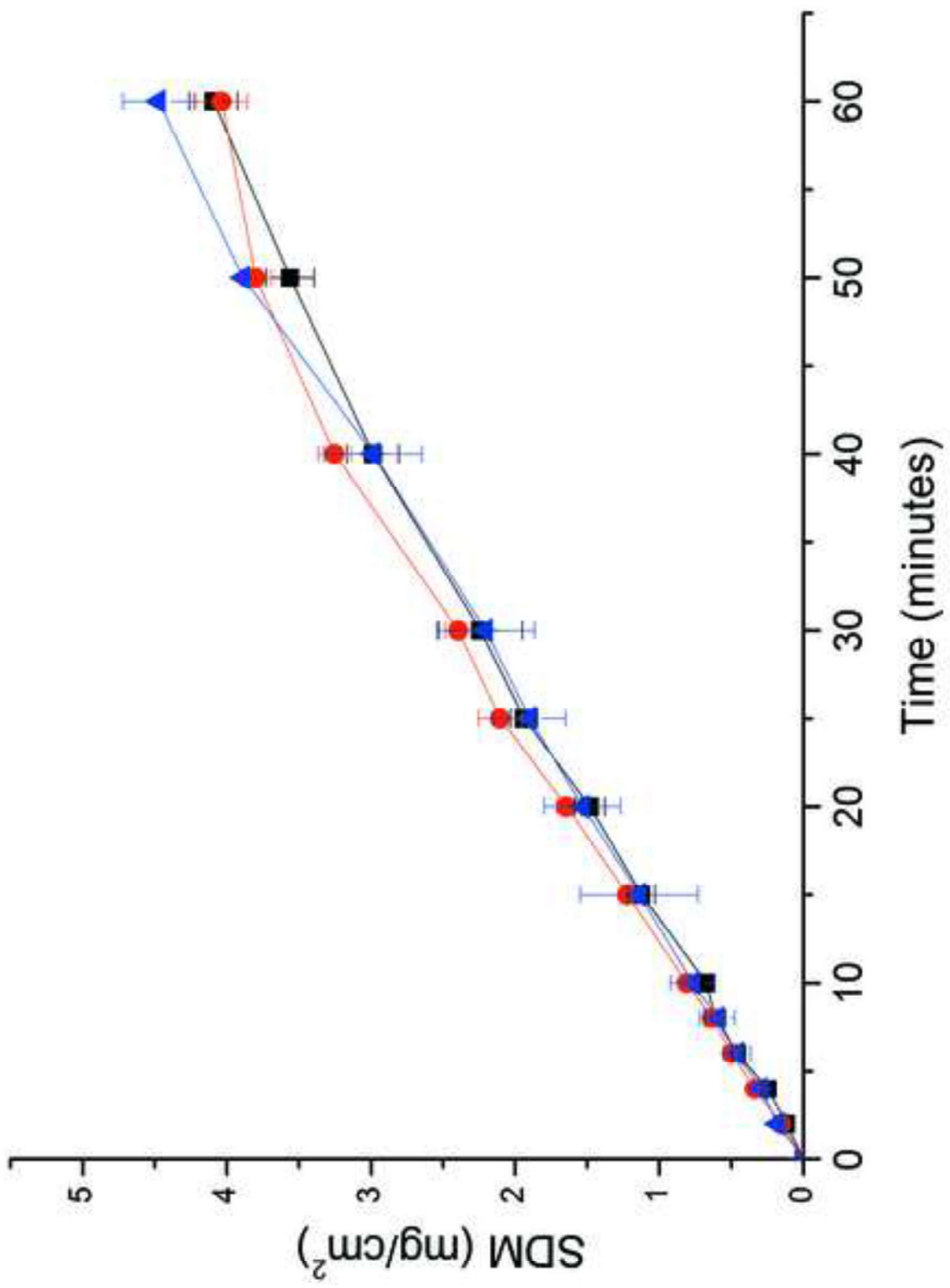


Figure 9

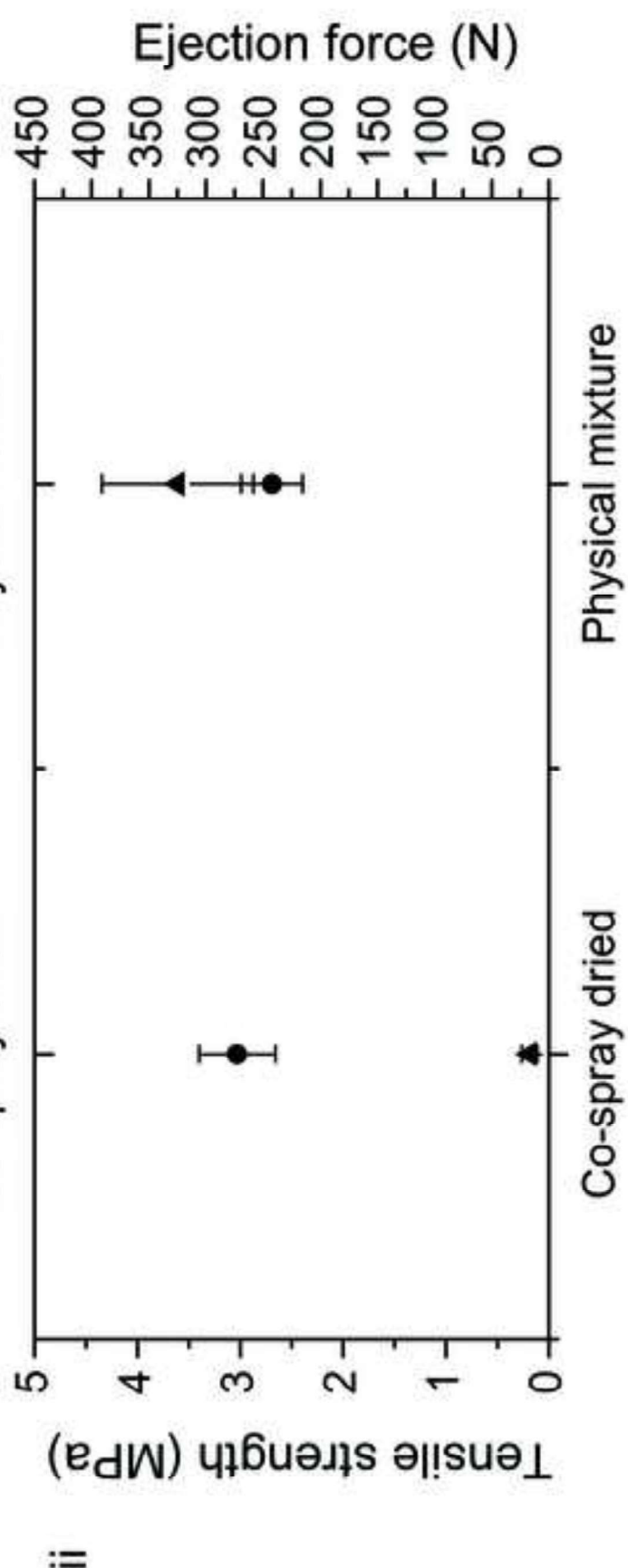
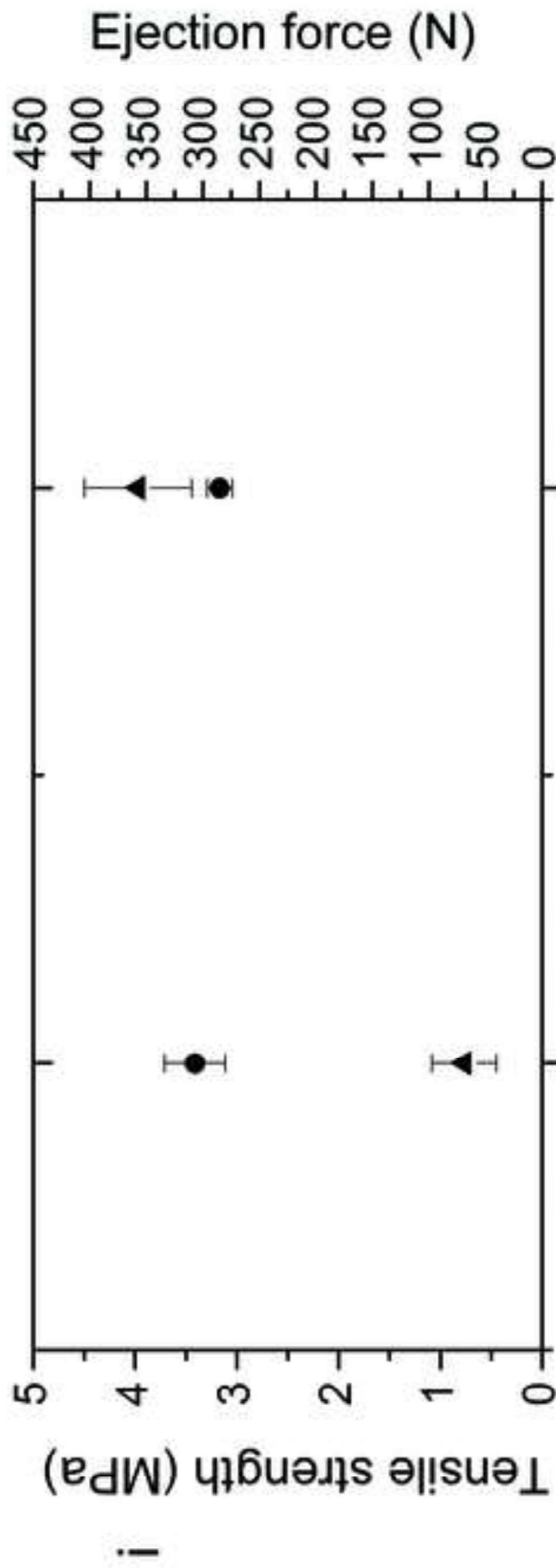


Figure 10